A MODIFIED RETINEX ILLUMINATION NORMALIZATION APPROACH FOR INFANT **PAIN RECOGNITION SYSTEMS**

MUHAMMAD NAUFAL BIN MANSOR MUHAMMAD NAUFAL BIN MANSOR

2014



A MODIFIED RETINEX ILLUMINATION NORMALIZATION APPROACH FOR INFANT PAIN RECOGNITION SYSTEM

MUHAMMAD NAUFAL BIN MANSOR (1140610592)

by

this item is pri A thesis submitted in fulfillment of the requirement for the Doctor of Philosophy

SCHOOL OF MECHATRONIC ENGINEERING **UNIVERSITI MALAYSIA PERLIS**

2014

UNIVERSITI MALAYSIA PERLIS

		DECLARATION OF THESIS		
Author's full name	: N	MUHAMMAD NAUFAL BIN MANSOR		
Date of birth	: 1	17/07/1983		
Title		A MODIFIED RETINEX ILLUMINATION NORMALIZATION APPROACH ANT PAIN RECOGNITION SYSTEM		
Academic Session	: 1	1/2014		
I hereby declare that that the library of UniMA		ecomes the property of Universiti Malaysia Perlis (UniMAP) and to be placed sis is classified as:		
CONFIDENTI	AL ((Contains confidential information under the Official Secret Act 1972)		
RESTICTED	-	(Contains restricted information as specified by the organization where research was done)		
	OPEN ACCESS I agree that my thesis is to be made immediately available as hard copy or on-line open access (full text)			
		the UniMAP to reproduce this thesis in whole or in part for the purpose of only (except during a period of years, if so requested above).		
		Certified by:		
. ?	rel			
SIGNA	ATURE	SIGNATURE OF SUPERVISOR		
830717-0 (NEW IC NO.)		PROF.DR.SAZALI YAACOB NAME OF SUPERVISOR		
Date: 10/09/	/14	Date: 10/09/14		

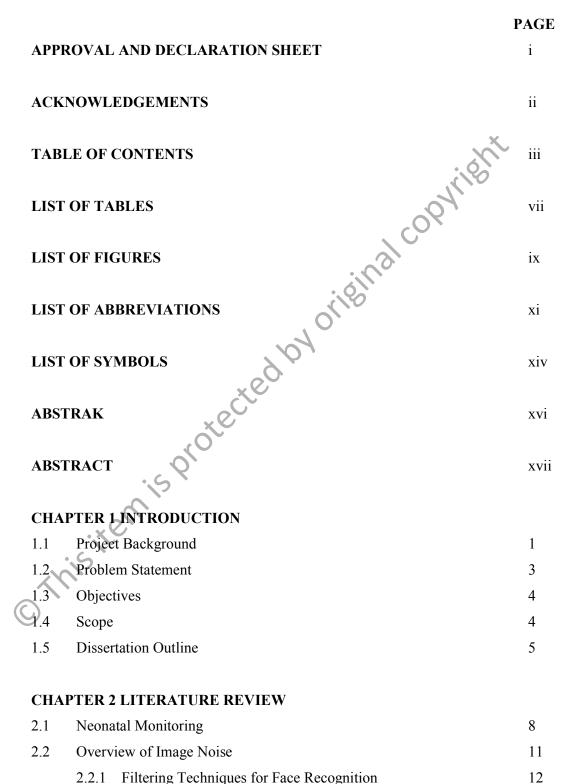
ACKNOWLEDGMENTS

I am very thankful to a number of people in seeing the successful completion of this work. First, I would like to thank Allah S.W.T for the endless blessings and gifts He has bestowed upon me. Without His blessing love, comfort, and guidance, not to mention answered prayers, I would never have made it to this point in my life.

I am in deep gratitude for the guidance and support of my academic advisor, Prof. Dr. Sazali Yaacob. He took me to work under him, provided me with a thesis topic and the necessary funds for my continuous effort. His thoughtful and insightful feedback throughout the semesters, challenge my work and bring it to this higher level of completion. I also extend a heartfelt thanks to Dr. M. Hariharan and Dr. Shafriza Nisha Basah. They worked hand in hand with me in experiments and helped me to maintain some form of sanity throughout endless experimental problems. Without their help, I would still be trying to figure out the robust analysis portion of this research. I will treasure them most and ever. I am also grateful to all of my colleagues particularly from Universiti Malaysia Perlis and Politeknik Tuanku Syed Sirajuddin for the opportunities to exchange ideas and diverse points of view at the group meetings. Special thanks also go to Ahmed Salah Eldin Mohammed Elsayed, Belinda Schwerin and Vitomir Struc for their valuable help, constructive feedback and cooperation. Without them none of this was possible.

My deepest gratitude goes to those people who are the most important in my life. My family, my wife, Azrini Idris, our sons Ammar and Amsyar for being supportive and encouraging over these years. To them I dedicate this dissertation.

TABLE OF CONTENTS



	e	1	e	
2.3	Preprocessing for Face	Recognition		13

	2.4	Illumi	nation Normalization Method for Face Recognition	13
	2.5	Histog	gram Normalization Method	14
		2.5.1	Histogram Equalization (HQ)	15
		2.5.2	Histogram Truncation and Stretching (HT)	16
		2.5.3	Normal Distribution (ND)	17
		2.5.4	Lognormal Distribution (LN)	18
		2.5.5	Extreme Value Distribution (EV)	19
		2.5.6	Exponential Distribution (EN)	20
	2.6	Photo	metric Normalization Method	21
		2.6.1	Single Scale Retinex (SSR)	21
		2.6.2	Homomorphic Filtering (HOMO)	23
		2.6.3	Exponential Distribution (EN) metric Normalization Method Single Scale Retinex (SSR) Homomorphic Filtering (HOMO) Single Scale Self Quotient Image (SSQ) Gross and Braiovic Technique (GBT)	24
		2.6.4	Gross and Brajovic Technique (GBT)	25
		2.6.5	DCT-Based Normalization (DCT)	27
		2.6.6	The Gradientfaces-based normalization technique (GRF)	28
		2.6.7	The Large-and Small-Scale Features Normalization Technique (LSSF)	30
		2.6.8	The Tan and Triggs Normalization Technique (TT)	31
	2.7	Featur	e Extraction of Infant Pain Images	32
		2.7.1	Correlation	33
		2.7.2	Principal Component Analysis	33
		2.7.3	Linear Discriminant Analysis	34
		2.7.4	Independent Component Analysis	35
	2.8	Classi	fication of Infant Pain Recognition Scheme	35
	X	2.8.1	k-Nearest Neighbor (kNN)	36
6		2.8.2	Artificial Neural Network (ANN)	36
6	9	2.8.3	Support Vector Machine (SVM)	37
	2.9	Propo	sed Approaches for Infant Pain Recognition System	37
	2.10	Summ	hary	39

CHAPTER 3 INFANT PAIN SYSTEMS AND PREPROCESSING

3.1	System Overview	41
3.2	Infant Cope Database (COPE)	43
	3.2.1 Subjects	43

		3.2.2	Procedure	44
	3.3	Grays	cale Image Representation	46
	3.4	Noise Image Representation		46
	3.5	Illumination Invariant Representation		47
	3.6	Propos	sed Preprocessing Method	49
		3.6.1	Median Filter	49
		3.6.2	Adaptive Filter	50
		3.6.3	Proposed Adaptive Median Filter	51
		3.6.4	Simulation Results	54
			3.6.4.1 Peak Signal-to-Noise Ratio (PSNR) Analysis	56
			3.6.4.2 Average Peak Signal-to-Noise Ratio (PSNR) Analysis	61
			3.6.4.3 Mean Square Error (MSE) Analysis	62
			3.6.4.4 Average Mean Square Error (MSE) Analysis	67
			3.6.4.5 Image Enhancement Factor (IEF) Analysis	68
			3.6.4.6 Average Image Enhancement Factor (IEF) Analysis	73
			3.6.4.7 Mean Structural SIMilarity (MSSIM) Index Analysis	74
			3.6.4.8 Average Mean Structural SIMilarity (MSSIM) Index Analysis	79
		3.6.5	The Modified Retinex Theory Normalization Technique	80
		3.6.6	Histogram Equalization (HQ)	85
	3.7	Summ	ary S	90
	CHAI	PTER 4	FEATURE SELECTION AND CLASSIFIER	
	4.1	Introd		91
	4.2	Princip	pal Component (PC) for Various Illumination and Noise Levels	92
(4.3		Binary Pattern (LBP) Parameter for Various Illumination and Levels	96
	4.4		ete Cosine Transform (DCT) Coefficients for Various Illumination oise Levels	101
	4.5	Propos	sed Features for Various Illumination and Noise Levels	105
	4.6	Classi	fication of Proposed Features	106
		4.6.1	k-Nearest Neighbor (kNN)	107
		4.6.2	Linear Discriminant Analysis (LDA)	108
		4.6.3	Artificial Neural Network (ANN)	109
			4.6.3.1 Multilayer Perceptron Neural Network (MLP)	110

		4.6.3.2 Probabilistic Neural Network (PNN)	111
		4.6.3.3 General Regression Neural Network (GRNN)	112
	4.6.4	Support Vector Machine (SVM)	113
		4.6.4.1 Outline of SVM	114
	4.6.5	Fuzzy k-Nearest Neighbor (F-kNN)	116
4.7	Sumn	nary	117

CHAPTER 5 PERFORMANCE ANALYSIS OF VARIOUS ILLUMINATION

LEVELS

	LEVE	LS	
	5.1	Introduction	118
	5.2	Performance Results under 25δ Illumination Levels with 10% Noise Level	128
	5.3	Average Performance Results under 25δ Illumination Levels with 10% Noise Level	133
	5.4	Performance Results under 50 δ Illumination Levels with 10% Noise Level	142
	5.5	Average Performance Results under 50δ Illumination Levels with 10% Noise Level	147
	5.6	Performance Results under 758 Illumination Levels with 10% Noise Level	156
	5.7	Average Performance Results under 75 δ Illumination Levels with 10% Noise Level	160
	5.8	Performance Results under 100δ Illumination Levels with 10% Noise Level	169
	5.9	Average Performance Results under 100δ Illumination Levels with 10% Noise Level	174
	5.10	Summary	175
0	СНАР	TER 6 CONCLUSION AND FUTURE WORK	
	6.1	Conclusion	177
	6.2	Future Work	179
	REFE	RENCES	181
	A DDF	NDIX A (List of publication)	101

AFFENDIA A (List of publication)		191
APPENDIX B (Performance Results (Table))	196

LIST OF TABLES

	NO.		PAGE
	3.1	PSNR for Various Filters for the Infant COPE Database at Different Noise Densities under 25 δ Illumination Levels	56
	3.2	PSNR for Various Filters for the Infant COPE Database at Different Noise Densities under 50 δ Illumination Levels	57
	3.3	PSNR for Various Filters for the Infant COPE Database at Different Noise Densities under 75 δ Illumination Levels	58
	3.4	PSNR for Various Filters for the Infant COPE Database at Different Noise Densities under 100δ Illumination Levels	59
	3.5	MSE for Various Filters for the Infant COPE Database at Different Noise Densities under 25 δ Illumination Levels	62
	3.6	MSE for Various Filters for the Infant COPE Database at Different Noise Densities under 50 δ Illumination Levels	63
	3.7	MSE for Various Filters for the Infant COPE Database at Different Noise Densities under 75 δ Illumination Levels	64
	3.8	MSE for Various Filters for the Infant COPE Database at Different Noise Densities under 100δ Illumination Levels	65
	3.9	IEF for Various Filters for the Infant COPE Database at Different Noise Densities under 25 δ Illumination Levels	68
	3.10	IEF for Various Filters for the Infant COPE Database at Different Noise Densities under 50 δ Illumination Levels	69
	3.11	IEF for Various Filters for the Infant COPE Database at Different Noise Densities under 75 δ Illumination Levels	70
	3.12	IEF for Various Filters for the Infant COPE Database at Different Noise Densities under 100δ Illumination Levels	71
6	3.13	MSSIM for Various Filters for the Infant COPE Database at Different Noise Densities under 25 δ Illumination Levels	74
6	3.14	MSSIM for Various Filters for the Infant COPE Database at Different Noise Densities under 50 δ Illumination Levels	75
	3.15	MSSIM for Various Filters for the Infant COPE Database at Different Noise Densities under 75 δ Illumination Levels	76
	3.16	MSSIM for Various Filters for the Infant COPE Database at Different Noise Densities under 100δ Illumination Levels	77
	4.1	Different PC for the Infant COPE Database at Different Noise Densities under 25 δ Illumination Levels	94
	4.2	Different PC for the Infant COPE Database at Different Noise Densities under 50 δ Illumination Levels	95

4.	3	Different PC for the Infant COPE Database at Different Noise Densities under 75 δ Illumination Levels	95
4.	4	Different PC for the Infant COPE Database at Different Noise Densities under 100δ Illumination Levels	95
4.	5	Different LBP Parameter for the Infant COPE Database at Different Noise Densities under 25δ Illumination Levels	99
4.	6	Different LBP Parameter for the Infant COPE Database at Different Noise Densities under 50 δ Illumination Levels	99
4.	7	Different LBP Parameter for the Infant COPE Database at Different Noise Densities under 75 δ Illumination Levels	100
4.	8	Different LBP Parameter for the Infant COPE Database at Different Noise Densities under 100δ Illumination Levels	100
4.	9	Different DCT Coefficients for the Infant COPE Database at Different Noise Densities under 25δ Illumination Levels	103
4.	10	Different DCT Coefficients for the Infant COPE Database at Different Noise Densities under 50 δ Illumination Levels	103
4.	11	Different DCT Coefficients for the Infant COPE Database at Different Noise Densities under 75 δ Illumination Levels	103
4.	12	Different DCT Coefficients for the Infant COPE Database at Different Noise Densities under 100δ Illumination Levels	104
4.	13	Comparison of Combination Features with Different Features for the Infant COPE Database at Different Noise Densities under 25δ Illumination Levels	105
4.	14	Comparison of Combination Features with Different Features for the Infant COPE Database at Different Noise Densities under 50δ Illumination Levels	105
4.	15	Comparison of Combination Features with Different Features for the Infant COPE Database at Different Noise Densities under 75 δ Illumination Levels	105
4	16	Comparison of Combination Features with Different Features for the Infant COPE Database at Different Noise Densities under 100δ Illumination Levels	106
5.	1	Performance Results under 25 δ Illumination Levels with 10% Noise Level	121
5.	2	Performance Results under 50 δ Illumination Levels with 10% Noise Level	135
5.	3	Performance Results under 75 δ Illumination Levels with 10% Noise Level	149
5.	4	Performance Results under 100δ Illumination Levels with 10% Noise Level	162

LIST OF FIGURES

N	O .	PAGE
2.	1 The Histogram Equalization (HQ) Technique .	16
2.2	2 The Histogram Truncation and Stretching (HT) Technique	e 17
2.	3 The Histogram Normal Distribution (ND) Technique	18
2.4	4 The Histogram Lognormal Distribution (LN) Technique	19
2.:	5 The Histogram Extreme Value Distribution (EV) Techniq	ue 19 20 23 23 24 25
2.0	6 The Single Scale Retinex (SSR) Technique	23
2.7	7 Homomorphic Filtering (HOMO) Block Diagram	23
2.8	8 Homomorphic Filtering (HOMO) Technique	24
2.9	9 Single Scale Self Quotient Image (SSQ) Technique	25
2.	10 Gross and Brajovic Technique (GBT)	26
2.	11 DCT-Based Normalization (DCT) Technique	27
2.	12 The Gradientfaces-Based Normalization Technique (GRF)) 30
2.	13 The Large-and Small-Scale Features Normalization Techr	nique (LSSF) 31
2.	14 The Tan and Triggs Normalization Technique	32
3.	1 The Proposed Study Procedure	42
3.2	2 The Infant COPE Database	44
3.	3 The Infant COPE Grayscale Image	46
3.4	4 Examples of the Different Noise Levels Effects	47
3.:	5 Examples of the Various Illuminations Level Image	48
3.0	6 Examples of the Effects of the Different Filter Methods	53
3,	7 Average Peak Signal-to-Noise Ratio (PSNR) Analysis	61
3.	8 Average Mean Square Error (MSE) Analysis	67
3.9	9 Average Image Enhancement Factor (IEF) Analysis	73
3.	10 Average Mean Structural SIMilarity (MSSIM) Analysis	79
3.	11 The Histogram Equalization (HQ) Image	87
3.	12 The Proposed Method Image	88
3.	13 Examples of the Effects of the Different Preprocessing Me	ethods 89
4.	1 The Infant COPE Database Eigen Face	94
4.2	2 The basic LBP Operator	96
4.	3 The Infant COPE LBP Image	98

4.4	The Infant COPE DCT Image	102
5.1	Average Performance Results under 25δ Illumination Levels with 10% Noise Level	133
5.2	Average Performance Results under 50 δ Illumination Levels with 10% Noise Level	147
5.3	Average Performance Results under 75 δ Illumination Levels with 10% Noise Level	160
5.4	Average Performance Results under 100δ Illumination Levels with 10% Noise Level	174
	Average Performance Results under 100 & Illumination Levels with 10% Noise Level	
© Ì		

LIST OF ABBREVIATIONS

	AC	Accuracy
	AMF	Adaptive Median Filter
	ANN `	Artificial Neural Networks
	AUC	Area under Curve
	CDF	Cumulative Distribution Function
	CONV	Conventional Validation
	COPE	Classification of Pain Expressions
	CRIES	Assesses Crying, Oxygen Requirement, Increased Vital Signs,
		Facial Expression, Sleep.
	CROSSV	Cross Validation
	DCT	DCT-Based Normalization
	DCT	Discrete Cosine Transform
	DOG	Difference of Gaussians
	ELBP	Elongated Binary Pattern
	ELTP	Elongated Ternary Pattern
	EN	Exponential Distribution
	EV	Extreme Value Distribution
	FFNN	Feed Forward Neural Network
	F-KNN	Fuzzy- k-Nearest Neighbor
	FM	F-Measure
	FN .	False Negative
	FP	False Positive
(GBT	Gross and Brajovic Technique
	GRF	Gradientfaces-Based Normalization Technique
	GRNN	General Regression Neural Network
	HCI	Human Computer Interface
	НОМО	Homomorphic Filtering
	HQ	Histogram Equalization
	HT	Histogram Truncation and Stretching
	IDCT	Inverse Discrete Cosine Transform
	IEF	Image Enhancement Factor

K-NN	K-nearest neighbor
LBP	Local Binary Pattern
LDA	Linear Discriminant Analysis
LN	Lognormal Distribution
LSSF	Large- and Small-Scale Features Normalization Technique
LSVM	Linear Support Vector Machine
MAX	Median
MIN	Minimum Multilayer Perceptron Neural Network Modified Retinex Normalization Technique
MLP	Multilayer Perceptron Neural Network
MRT	Modified Retinex Normalization Technique
MSE	Mean Square Error
MSSIM	Mean Structural SIMilarity Index
NF	New Feature
ND	Normal Distribution
NICU	Neonatal Intensive Care Unit
NIPS	Neonatal Infant Pain Scale
NNSOA	Neural Network Simultaneous Algorithm
N-PASS	Neonatal Pain, Agitation and Sedation Scale
OSH	Optimal Separating Hyperplane
PCA	Principal Component analysis
PIPP	Premature Infant Pain Profile
PNN	Probabilistic Neural Network
PRE	Precession
PSNR S	Peak Signal-to-Noise Ratio
REC	Recall
SE	Sensitivity
SP	Specificity
SSIM	Structural SIMilarity Index
SSQ	Single Scale Self Quotient Image
SSR	Single Scale Retinex
SVM	Support Vector Machine
SVMLIN	SVM Linear kernel
SVMMLP	SVM MLP kernel
SVMPOL	SVM Polynomial kernel

SVMRBF	SVM RBF kernel
TN	True Negative
ТР	True Positive
TT	Tan and Triggs Normalization Technique

O This item is protected by original copyright

LIST OF SYMBOLS

I(x,y)	Image on (x,y) coordinate
J(i)	Probability image
\mathcal{U}_i	Number of pixels
i _{out}	Latest intensity value
g(x)	Allotment function order grouped Scale parameter Reflectance on (<i>x</i> , <i>y</i>)coordinat Illumination on (<i>x</i> , <i>y</i>)coordinat Non linear function Quotient images Weighting factors Scale Parameter
Κ	order grouped
β	Scale parameter
R(x,y)	Reflectance on (x,y) coordinat
L(x,y)	Illumination on (x,y) coordinat
Т	Non linear function
Qk	Quotient images
Mk	Weighting factors
k	Scale Parameter
WkGk	Weighted Gaussian kernels
G	Gradientfaces
δ	Delta factor
$\frac{1}{I}$	Gain
Ψ	Small neighborhood
Ω	Image domain
ρ	Anisotropic diffusion coefficients
2	Smoothness constraint
Ch l	Grid interval
\mathbb{C}_{f}^{h}	Ratio of total intensity difference
\hat{f}	Output Image
W	Current $N x N$ window centered at $g(x, y)$
m_L	Local Mean
Φ_i	Vector image
$\omega_{_k}$	Eigen-Vector
$B_{p,q}$	Weights functional

W_{opt}	Finest projection
x_L	Projected sets
Y^i	Observed values

orthis item is protected by original copyright

Pengubahsuaian Normalisasi Iluminasi Retinex dalam Pendekatan Mengesan Kesakitan pada Bayi

ABSTRAK

Kesakitan bayi dipantau di dalam Neonatal Jagaan Unit Rapi (NICU). Kesakitan pada bayi dapat dikesan dengan mengkaji perubahan mimik muka mereka. Walaupun keputusan yang diperolehi amat memberangsangkan, ianya tidak cukup dalam aspek gangguan dan perubahan iluminasi. Penyaring Penyesuai Median (AMF) untuk menapis gangguan telah dicadangkan. Purata dan varian nilai median digunakan untuk menghasilkan pemberat yang bersesuaian dengan imej menggunakan 3x3,5x5 or 7x7 telah digunakan. Keputusan kuantitif seperti Puncak Isyarat kepada nisbah gangguan (PSNR), Purata Kuasa Dua Ralat (MSE), Faktor Peninggian Imej (IEF) dan Indeks Persamaan Purata Struktur (MSSIM). Keputusan purata menunjukkan peningkatan dengan 40.63 db untuk PSNR, 6.01 untuk MSE, 258.09 untuk IEF dan 0.97 untuk MSSIM. Dalam kajian ini juga iluminasi normalisasi baru yang dikenali sebagai Pengubahsuaian Retinex Teknik (MRT) untuk mengesan muka dalam perbezaan iluminasi dengan menggabungkan normalisasi histogram dan gabungan kombinasi ciri telah dicadangkan. Kaedah ini telah dibandingkan dengan kaedah seperti (SSR) Skala Tunggal Retinex, (HOMO) Kaedah Homomorphic, (SSQ) Skala Tunggal Nisbah Imej, Gross dan Brajovic Teknik (GBT), (DCT) Kaedah DCT, (GRF) Teknik perubahan muka, (TT) Kaedah Tan dan Triggs, and Teknik Besar dan Kecil (LSSF) untuk menilai kecekapannya. Kaedah ini tidak memerlukan maklumat luaran tentang bentuk muka dan iluminasi malahan boleh digunakan pada stiap imej secara berasingan. Kajian dijalankan menggunakan imej COPB data. Keputusan yang ditunjukkan amat memberangsangkan. Pengambilan pencirian tunggal seperti Analisis Komponen Prinsipal (PCA), Corak Tempatan Dedua (LBP) dan Transformasi Sudut Berasingan (DCT) menghasilkan keputusan yang baik. Walaubagaimanapun gabungan ketiga-tiga pengambilan pencirian ini menghasilkan ketepatan yang amat memberangsangkan. Kaedah MRT bersama gabungan pengambilan pencirian mendapat keputusan >90% pada sepuluh klasifikasi seperti Jiran Terdekat K (k-NN), Fuzi Jiran Terdekat K (Fuzzy k-NN), Pembezaan Analisis Lurus (LDA). Masukan Terus Rangkaian Neural (FFNN). Kemugkinan Rangkaian Neural (PNN), Regresi Umum Rangkaian Neural (GRNN), Mesin Pembantu Wektor Lurus (SVMLIN), Mesin Pembantu Vektor Fungsi Asas Radial (SVMRBF), Mesin Pembantu Vektor Pelbagai Lapisan (SVMMLP) dan Mesin Pembantu Vektor polinomial (SVMPOL) dalam beberapa pengukuran prestasi seperti sensitivity, spesifikasi, ketepatan, luas bawah lengkung (AUC), Cohen's kappa (k), kepersisan, Pegukur F dan masa proses.

A Modified Retinex Illumination Normalization Approach for Infant Pain Recognition System

ABSTRACT

Pains in newborn babies are monitored in a Neonatal Intensive Care Unit (NICU) for medical treatment. Pain in newborns can be detected by studying their facial appearance. Even though the outcome is acceptable, it is not adequately vigorous to be used in unpredictable, non-ideal situations such as noise and varying illumination environment. First, to improve the noise cancellation robustness an adaptive median filter (AMF) is proposed. Mean and variance of median values are selected to generate a weight for each window part of the images such as 3x3, 5x5 or 7x7. Various linear and nonlinear filters are adopted to eliminate the noise in the images. Quantitative comparisons are performed between these filters with our AMF in terms of Peak Signal-to-Noise Ratio (PSNR), Mean Square Error (MSE), Image Enhancement Factor (IEF) and Mean Structural SIMilarity (MSSIM) Index. The average results show improvement in terms of 40.63 db for PSNR, 6.01 for MSE, 258.09 for IEF and 0.97 for MSSIM respectively. In this work a novel method of illumination invariant normalization known as Modified Retinex Normalization (MRT) for preprocessing of infant face recognition is proposed. This is based on a modified retinex model that combines with histogram normalization for filtering the illumination invariant. The proposed method is compared to other methods like Single scale Retinex (SSR), Homomorphic method (HOMO), Single Scale Self Quotient Image (SSQ), Gross and Brajovic Technique (GBT), DCT-Based Normalization (DCT), Gradientfaces-based normalization technique (GRF), Tan and Triggs normalization technique (TT), and Large-and small-scale features normalization technique (LSSF) for evaluation with Infant Classification of Pain Expressions (COPE) database. Several experiments were performed on COPE databases. Single PCA, LBP and DCT feature extraction information yielded a good recognition result. However, by summing these three, it gives more robustness to noise and illumination classification rate because the sum rule was the most resilient to estimate errors and gives higher than 90% accuracies of pain and no pain detection. The new illumination normalization and combination of features gives higher results of more than 90% on five different elassifiers with various algorithms such as k-nearest neighbors (k-NN), Fuzzy k-nearest neighbors (FkNN), Linear Discriminat Analysis (LDA), Feed Forward Neural Network (FFNN), Probabilistic Neural Network (PNN), General regression Neural Network (GRNN), SVM Linear kernel (SVMLIN), SVM RBF kernel (SVMRBF), SVM MLP kernel (SVMMLP) and SVM Polynomial kernel (SVMPOL) with different performance measurement such as Sensitivity, Specificity, Accuracy, Area under Curve (AUC), Cohen's kappa (k), Precession, F-Measure and Time Consumption.

CHAPTER 1

INTRODUCTION

1.1 Project Background

Newborn babies are monitored in a Neonatal Intensive Care Unit (NICU) for medical treatment include perinatal asphyxia, major birth defects, sepsis, neonatal, and Infant respiratory distress syndrome due to immaturity of the lungs. These infants are nurtured in an incubator, where their vital bodily function indicators such as blood pressure, temperature, heart rate, oxygen concentration and respiration are continuously observed. To avoid disturbed sleep caused by bright lights which leads to anxiety, the incubator is covered with a blanket to reduce the intensity of light. The drawback of this practice is that visual inspection of the infant throughout most of the time is impaired. In other words, ache and distress cannot be assessed by observing crucial functions. There are growing concerns that early detection of pain and distress may be important for the infant's development which prompts us to widen a model for an automated video surveillance system that can detect ache and distress in neonates.

Distress in newborns can be detected by studying their facial appearance (Grunau et al., 1987; Stevens et al., 1996; Chen et al., 2005). In particular, the appearance of the mouth, eyebrows and eyes are reported to be significant facial features for detecting the occurrence of distress and ache. This has resulted in the development of scoring systems to evaluate the intensity of distress, based on facial appearance and physiological

parameters. The scoring systems provide early signals to care takers when newborns experience ache or distress, so proper actions can be taken in an instant.

So far, only one automatic video-surveillance system (Brahnam et al., 2006; Brahnam et al., 2007) for pain detection in newborn babies has been reported. In this system, enlarged images of an infant are taken in diverse situations: using a painful method (heel lance) and during other non-painful situations such as friction, crying, resting and air stimulus. After manual rotation and scaling, pixel-based classifiers, such as Linear Discriminant Analysis and Support Vector Machines (Brahnam et al., 2006; Brahnam et al., 2007; Martinez & Kak, 2004; Abdi, 2007; Perriere & Thioulouse, 2003) were applied for sorting the facial expressions. Even though the outcome is acceptable, it believe that this is not adequately vigorous to be used in unpredictable, non-ideal situations such as under varying noise and illumination environment, where the newborn's face is partly covered by plasters or tubing.

Illumination is one of the basic characteristics of a visible surface and it provides information for scene interpretation (Gao et al., 2003; Chen et al., 2000). Recent developments in this field have shown that there is room for improvements. Most of the traditional face recognition algorithms are satisfactory under controlled conditions. However, when dealing with performance degrading issues such as variation in pose, noise, illumination, and facial expression, their accuracy greatly diminished (Gao et al., 2003; Chen et al., 2000). As the performance of a face recognition technique is significantly affected by various illumination and noise effects, illumination and noise are known to be the key factors that play an important role in human face recognition system design.

To address this limitation, this dissertation proposed a distress detection scheme and depicts a pilot method with the following properties: first, the identification of distress will be based on analyzing the whole face region in an automated way. With this information, the behavioral circumstances of the infant either in pain or normal can be detected. Images of surrounding factors such as the visibility of plasters and tubes on the infant are excluded in this work. However, other challenging circumstances, such as the changes in noise and illumination environment, which characteristically lead to risinal copy suboptimal surroundings, need to be considered.

1.2 **Problem Statement**

Many issues hinder research efforts in the field of infant face recognition. Variation exists in every imaging approaches, and finding fast, simple algorithms that are robust to variation is difficult (Brahnam et al., 2006; Brahnam et al., 2007). Categorizing the variation may be helpful in the development of effective face recognition algorithms (Matthew, 2003). Intrinsic sources of variation include identity, facial expression, speech, gender, and age (Daugman, 1997). Extrinsic sources of variation include viewing geometry pose changes, illumination (shading, color, self-shadowing), imaging processes (resolution, focus, imaging noise), and other objects (occlusions, shadowing, and indirect illumination).

These sources of variation may or may not hinder the recognition process depending on the algorithm used. It is possible that the variation due to factors such as facial expression, lighting, occlusions, noise and pose is larger than the variation due to identity (Daugman, 1997). That makes identification under such varying environments a

difficult task. However, human proficiency at face recognition (Hochberg et al., 1967) has motivated enormous research in this area despite these challenges. Thus, this work seeks to solve the problems of infant face recognition system in different noise levels and illumination with new filter and new illumination normalization approach.

1.3 Objectives

The objectives of this research are as follows:

- To develop a new approach based on filter under varying conditions of noise level in preprocessing phase.
- To develop a new illumination normalization approach under varying conditions of illumination level.
- To determine the most salient and discriminative features by adopting the feature selection for optimizing on the accuracy of the decision making systems.
- 4) To evaluate the performance of the new illumination normalization method for detecting illumination invariant capability in terms of sensitivity, specificity, accuracy, area under curve, Cohen's kappa, precession, recall, fmeasure and execution time under different noise and illuminations levels.

1.4 Scope

As mentioned in the introduction, it seems not much attention is given to research on monitoring of infants in Neonatal Intensive Care Units (NICU). This work may answer many of the misconceived problems. In this work, one approach to Human Computer Interface (HCI) for monitoring infant pain is presented. Most of the infants represent their pain through their facial appearance, and hence monitoring the whole body movement is not a viable solution. The facial appearance need to be monitored by the nurses at selected intervals and reported to doctors for possible further treatments. Detection of facial changes is very crucial for further treatment. This work is only limited to the face from infant COPE database. The database of whole images in this work only consists of upfront images and does not deal with different poses. Within this work, only common features such as PCA, LBP and DCT are adopted. However, different parameters and coefficient of features under different illumination levels and noise are adopted. Salt and pepper noise is employed rather than other noise because this type of noise always appears in digital images and is mostly adopted as a benchmark for filter performance evaluation. The proposed filter is tested with various quantitative measurements such as Peak Signal-to-Noise Ratio (PSNR), Mean Square Error (MSE), Image Enhancement Factor (IEF) and Mean Structural SIMilarity (MSSIM) Index. In this work, selected noise and illumination levels on the face of infant is investigated. Certain performance measurement such as Sensitivity, Specificity, Accuracy, Area under Curve (AUC), Cohen's kappa (k), Precession, F-Measure and Time Consumption are measured to validate the proposed illumination normalization technique.

1.5 Dissertation Outline

The chapters of this dissertation largely follow the order in which the work was done. The scope and objective of the work is presented in this chapter. The second chapter is a literature review encompassing most of infant monitoring research. This