

## DEVELOPMENT OF SHEAR HORIZONTAL SURFACE ACOUSTIC WAVE WITH SILICON DIOXIDE NANOPARTICLES WAVEGUIDE SENSOR FOR ESCHERICHIA COLI 0157:H7 DETECTION

by

# TEN SENG TEIK 1241710767

A thesis submitted in fulfilment of the requirements for the degree of Doctor of Philosophy

> Institute of Nano Electronic Engineering UNIVERSITI MALAYSIA PERLIS

> > 2017

### UNIVERSITI MALAYSIA PERLIS

DECLARATION OF THESIS			
Author's full name	:	TEN SENG TEIK	
Date of birth	:	13 APRIL 1974	
Title	:	DEVELOPMENT OF SHEAR HORIZONTAL SURFACE ACOUSTIC WAVE WITH SILICON DIOXIDE NANOPARTICLES WAVEGUIDE SENSOR FOR <i>ESCHERICHIA COLI</i> 0157:H7 DETECTION	
Academic Session	:	2016/2017	
I hereby declare that the thesis becomes the property of Universiti Malaysia Perlis (UniMAP) and to be placed at the library of UniMAP. This thesis is classified as:			
CONFIDENTIA	L	(Contains confidential information under the Official Secret Act 1972)*	
RESTRICTED		(Contains restricted information as specified by the organization where research was done)*	
OPEN ACCESS		I agree that my thesis is to be made immediately available as hard copy or on-line open access (full text)	
I, the author, give permission to the UniMAP to reproduce this thesis in whole or in part for the purpose of research or academic exchange only (except during a period of years, if so requested above).			
	n'is'	Certified by:	
SIGNAT	FURE	SIGNATURE OF SUPERVISOR	
(NEW IC NO./ P	<u>7-5021</u> ASSPOF	RT NO.) <u>PROF. DR. UDA BIN HASHIM</u> NAME OF SUPERVISOR	
Date:		Date:	

#### ACKNOWLEDGEMENT

The author could not have accomplished these studies without the help of God and many great people. First, the author would like to express his deep gratitude to his main project supervisor, Prof. Dr. Uda bin Hashim, his supervisory committee, Assoc. Prof. Dr. Anis Nurashikin binti Nordin, and Dr. Liu Wei Wen for their valuable advice, guidance, and willingness to share their expertise.

The author would like to thank MARDI for the sponsorship and the opportunity to complete his thesis, and Ahmad bin Sudin, the project leader of Nano Science Fund, for financially supporting this research. The author is also indebted to Dr. Foo Kai Loong for his great support, Dr. Ramzan Mat Ayub, Dr. Mohd Khairuddin Md Arshad, Dr. Subash C. B. Gopinathhe, Dr. Joanne Edmondston (UWA), Dr. Wilson (NASA), Dr. Voon Chun Hong, Dr. Wee Fwen Hoon, Dr. Mohammad Nuzaihan Md Nor, Jasni Mohamed Ismail, Mohammad Isa Ahmad Azan, Nur Shamira Shohaimi, Mohd Aizat bin Abdul Rane, Yeng Seng, Guat Yee, Tze Qing, and Wai Hoong for providing the equipment, insight, guidance, and aid to carry out this project.

Special thanks to Tiek Aun, Hui Yen, Mohamad Faris, Humaira, Surai, Siti Fatimah, Fatin Nabilah, Sharipah, Nor Azizah, Adelyn Puah, Hasrul Hisham, Hon Cheun, Adzhri, among others for providing moral support during tough times. The author would also like to acknowledge the help of Alan Gooi for the instrumental support.

The author would like to express his deepest gratitude to his dearest parents, dearest brother and sister-in-law, and all relatives for their encouragement and support. The author is also very much indebted to his dearest loving wife for walking side by side patiently and supportively throughout his studies and for also taking care of the family well. The author is also grateful to his children for accompanying and bringing joy to him. The author couldn't have done it without the great support from his family.

Last but not least, the author appreciates the help from the people around him throughout the study.

### TABLE OF CONTENTS

	PAGE
DECLARATION OF THESIS	i
ACKNOWLEDGEMENT	ii
TABLE OF CONTENTS	iii
LIST OF FIGURES	vii
LIST OF TABLES	xii
LIST OF ABBREVIATIONS	xiv
LIST OF SYMBOLS	xvii
ABSTRAK	XX
ABSTRACT	xxi
CHAPTER 1 INTRODUCTION	1
1.1 Introduction	1
1.2 Problem Statement	5
1.3 Research Objectives	6
1.4 Research Scopes	7
1.5 Contributions	9
(1.6 Thesis Organisation	9
CHAPTER 2 LITERETURE REVIEW	11
2.1 Introduction	11
2.2 Acoustic based devices	11
2.2.1 Bulk acoustic wave	14
2.2.1.1 Thickness Shear Mode	14

2.2.1.2 Thin-Film Thickness-mode Bulk Wave	16
2.2.1.3 Shear Horizontal Acoustic Plate Mode	17
2.2.2 Surface Acoustic Waves	19
2.2.2.1 Rayleigh wave	20
2.2.2.2 Shear Horizontal Surface Acoustic Wave (SHSAW)	22
2.2.2.3 Surface Skimming Bulk-Wave (SSBW)	23
2.2.2.4 Surface Transverse Wave	23
2.2.2.5 Love Wave	25
2.2.3 Plate Wave	27
2.3 Comparison of Acoustic Based Sensors Sensitivity	31
2.4 SAW Devices Modeling Methods	33
2.4.1 Mathematical Related Circuit Response Models	33
2.4.1.1 Early Analytic Methods for SAW Filter Circuit-Design Models	34
2.4.1.2 Current Analytic Methods for SAW filter Circuit-Design Model	35
2.4.2 Finite Element Method for SAW Devices	37
2.4.3 SAW Related Modelling Equations	38
2.5 Design Experiment for SHSAW IDT Development	42
2.6 SAW Device Fabrication Methods	45
2.6.1 Metal Deposit Methods	45
2.6.2 Lithography methods	46
2.6.3 IDT Design	48
2.6.4 SAW Device Fabrication Materials	50
2.7 Silicon Oxides Thin Film Deposition Methods	53
2.8 Silicon oxides Surface Functionalization	56

2.9	Chapter Summary	60
CHAPTER	3 METHODOLOGY	61
3.1	Introduction	61
3.2	SHSAW Modeling Method	61
3.3	Fabrication of SHSAW Devices	66
	3.3.1 IDT Design	66
	3.3.2 IDTs Fabrication	68
3.4	Investigate and Identify the Effect of IDT on Mass Loading Sensitivity through Experiment	75
	3.4.1 Design of Experiments in IDT Parameters Study	76
	3.4.2 Experiment Setup in IDT Parameters Study	78
3.5	Development of SiO2 Nanoparticles Waveguide SHSAW Sensor for <i>E.coli</i> O157:H7 DNA Detection	80
	3.5.1 Fabrication of SiO2 Nanoparticles Thin Film Waveguide	80
	3.5.2 Functionalization SiO2 Nanoparticles Thin Layer Waveguide Surface for DNA Detection	82
	3.5.3 Characterization of SiO2 Nanoparticles Waveguide Biosensor	87
3.6	Chapter Summary	88
CHAPTER	4 RESULTS AND DISCUSSION	89
4.1	Introduction	89
4.2	SHSAW Modelling Evaluations	89
4.3	Fabrication of SHSAW Devices Evaluations and Discussion	97
4.3	9.1 Physical Fabrication Results	98
4.3	E.2 Electrical Measurement Results	102
4.4	Analysis the Effect of IDT on Mass Loading Effect Sensitivity by RSM	111

4.4.1 RSM Model Evaluation	111
4.4.2 Effect of IDT Parameters on Resonant Frequency Shifting with The Temperature Effect	116
4.4.3 Effect of IDT Parameters on Resonant Frequency Shifting with The Mass Loading Effect	118
4.4.4 Identify of the Most Sensitive Fabricated Device for Biosensor Purpose	127
4.5 Evaluation of SiO2 Nanoparticles Waveguide SHSAW Sensor for E.coli O157:H7 DNA Detection	128
4.5.1 Evaluation of SiO2 Nanoparticles Waveguide Deposition	129
4.5.2 Evaluation of Surface Modification and Functionalization	132
4.5.3 Analytical Performance of SiO2 Nanoparticles Waveguide Biosensor	136
4.6 Chapter Summary	143
CHAPTER 5 CONCLUSION AND FUTURE WORK	144
REFERENCES	147
APPENDIX A: FREQUENCY SHIFT DIAGRAMS OF HYBRIDIZATION OF DIFFERENT CONCENTRATIONS TARGET DNA ON 12 µm ELECTRODE WIDTH	
SHSAW DEVICES	167
APPENDIX B: JOURNAL PUBLICATION	171
APPENDIX C: CONFERENCE PROCEEDING PUBLICATION	173
APPENDIX D: AWARDS	184

### LIST OF FIGURES

NO	PAGE
Figure 2.1: DNA sensing mechanism used in SAW DNA biosensor (Gronewold, 2007).	12
Figure 2.2: Two modes of wave propagations: (a) longitudinal and (b) transverse waves.	14
Figure 2.3: Types of acoustic waves.	15
Figure 2.4: AT-cut quartz QCM device.	16
Figure 2.5: Configuration of SH-APM sensor (Drafts, 2001).	18
Figure 2.6: Rayleigh wave propagation (Sankaranarayanan, 2007).	20
Figure 2.7: Wave energy is confined to within one wavelength from the surface (Drafts, 2001).	22
Figure 2.8: Delay line configurations of the STW (Vellekoop, 1998).	24
Figure 2.9: Trapping the wave energy in the surface by the metal grating in STW.	24
Figure 2.10: Scheme of a Love Wave device (Rocha-Gaso, et al., 2009).	26
Figure 2.11: Lamb wave modes: (a) symmetrical mode and (b) asymmetrical mode (Rocha-Gaso, et al., 2009).	28
Figure 2.12: Calculated phase velocity of different flexural plate wave modes over ratio of plate thickness, d, to wavelength, $\lambda$ , for silicon nitride (D. S. Ballantine et al., 1996).	29
Figure 2.13: Schematic cross-sectional view of the FPW sensor.	30
<ul><li>Figure 2.14: The configuration of Euler angles, (a) rotation about Z-axis,</li><li>(b) rotation about X'-axis, (c) rotation about Z'-axis.</li></ul>	41
Figure 2.15: Three main SAW IDT configurations.	48
Figure 3.1: Schematic of a two-port delay line SAW sensor model.	63
Figure 3.2: Design parameters of the SHSAW IDT.	64
Figure 3.3: Schematic of a two-port delay line SAW sensor with mass loading effect.	64

Figure 3.4: Overall lithography process for aluminum IDTs on 64 <sup>0</sup> YX LiNbO <sub>3</sub> .	70
Figure 3.5: Dropping of photoresist on the center of the sensing area of the devices for the $\Delta f$ measurement due to mass loading effect.	79
Figure 3.6: Instrument setup for measuring the resonant frequency change due to temperature effect.	80
Figure 3.7: SiO2 nanoparticles waveguide SHSAW device fabrication flow.	82
Figure 3.8: The flow chats of surface functionalization process and hybridization process.	85
Figure 3.9: The surface functionalization process including the surface modification steps from (a) SiO2 deposition, (b) APTES,	
(c) glutaraidenyde to (d) probe DNA immobilization processes and (e) DNA hybridization process on LiNbO3 substrate.	86
Figure 4. 1: Frequency versus output voltage signal obtained at output terminal of device no.1.	90
Figure 4.2: COMSOL simulation 3D plot surface displacement of device no.1 at resonant frequency response.	91
Figure 4.3: COMSOL simulation 3D plot surface displacement of device no.1 at non-resonant frequency response.	91
Figure 4.4: COMSOL simulation 3D plot surface displacement of device no.1 with mass loading effect at resonant frequency response.	92
Figure 4.5: Comparison of resonant frequency shift between for models with and without mass loading effect for device no. 1.	94
Figure 4.6: Comparison for effect of number of transmission and receiving IDT pairs toward the mass loading effect sensitivity.	95
Figure 4.7: Comparison for effect of metal strip overlap distance pairs toward the mass loading effect sensitivity.	95
Figure 4.8: Comparison for effect of delay line length toward the mass loading effect sensitivity.	97
Figure 4.9: 3 $\mu$ m strip width for 12 $\mu$ m pitch size device.	98
Figure 4.10: 8 $\mu$ m strip width for 32 $\mu$ m pitch size device.	99
Figure 4.11: 12 µm strip width for 48 µm pitch size device.	99

Figure 4.12: 15 $\mu$ m strip width for 60 $\mu$ m pitch size device.	100
Figure 4.13: 20 µm strip width and 80 µm pitch size.	100
Figure 4.14: Metal strip AFM thickness profile image.	102
Figure 4.15: Insertion loss plotting for 32 µm pitch size.	103
Figure 4.16: Insertion loss plotting for 48 µm pitch size.	104
Figure 4.17: Insertion loss plotting for 60 µm pitch size.	104
Figure 4.18: Insertion loss plotting for 80 µm pitch size.	105
Figure 4.19: 12 µm pitch size with SiO2 thin film coating.	105
Figure 4.20: Resonant frequency measurement for 8µm pitch sizes with various combinations of different pairs of input and output IDTs, aperture size and delay line length, (a) 50 pairs input and 50 pairs output IDTs, (b) 50 pairs input and 95 pairs output IDTs, (c) 95 pairs input and 50 pairs output IDTs and (d) 95 pairs input and 95 pairs output IDTs.	106
Figure 4.21: Resonant frequency measurement for 12µm pitch sizes with various combinations of different pairs of input and output IDTs, aperture size and delay line length, (a) 73 pairs input and 73 pairs output IDTs and (b) 2.88mm aperture and 8.4mm delay line length.	107
Figure 4.22: Resonant frequency measurement for 15µm pitch sizes with various combinations of different pairs of input and output IDTs, aperture size and delay line length, (a) 50 pairs input and 50 pairs output IDTs, (b) 50 pairs input and 95 pairs output IDTs, (c) 95 pairs input and 50 pairs output IDTs and (d) 95 pairs input and 95 pairs output IDTs.	108
Figure 4.23: Normal plot of residuals (a) and residuals versus predicted plot (b) for temperature effect.	114
Figure 4.24: Normal plot of residuals (a) and residuals versus predicted plot (b) for mass loading effect.	115
Figure 4.25: Temperature effect versus IDT pitch size.	117
Figure 4.26: Mass Loading effect versus IDT pitch size.	119
Figure 4.27: Mass loading versus (a) aperture, (b) delay line length for 8 μm pitch size devices.	120
Figure 4.28: Mass loading versus (a) aperture, (b) delay line length for 12 μm pitch size devices.	121

Figure 4.29: Mass loading versus (a) aperture, (b) delay line length for 15 μm pitch size devices.	122
Figure 4.30: Mass loading versus no. transmission IDT for 8 µm pitch size devices.	123
Figure 4.31: Mass loading versus no. transmission IDT for 12 µm pitch size devices.	124
Figure 4.32: Mass loading versus no. transmission IDT for 15 µm pitch size devices.	124
Figure 4.33: Mass loading versus no. receiving IDT for 8 µm pitch size devices.	125
Figure 4.34: Mass loading versus no. receiving IDT for 12 µm pitch size devices.	126
Figure 4.35: Mass loading versus no. receiving IDT for 15 µm pitch size devices.	126
Figure 4.36: Comparison mass loading sensitivity of the five different IDT parameters.	128
Figure 4.37: Design of the SiO2 nanoparticles wave guided SHSAW biosensor: (a) The final structure of fabricated biosensor for E. coli O157:H7 detection, (b) HPM image of center SiO2 deposited sensing area with APTES added, (c) the image of AFM image of SiO2 deposition surface. (d) The image of FESEM of the	
SiO2 nanoparticles at 5 kV with 800 000 magnification.	131
Figure 4.38: SiO <sub>2</sub> thickness obtained from RF sputtering.	132
Figure 4.39: Insertion loss against frequency after SiO <sub>2</sub> deposition.	132
Figure 4.40: Affirmation of SiO2 deposition: (a) EDX spectrum upon SiO2 deposition, (b) SiO2 compound confirmation by XRD.	134
Figure 4.41: Affirmation of surface functionalization layers through infrared spectrum scanning by FTIR upon every layer of surface modification process.	135
Figure 4.42: Resonant frequency shift of 32 µm pitch size device after hybridization process with 1µm concentration complementary target.	137
Figure 4.43: Comparison frequency shift by hybridization different complementary DNA concentration for 12 µm and 32 µm pitch IDTs.	140

Figure 4.44: Frequency shift response curve with different concentrations of <i>E. coli</i> O157:H7 DNA.	141
Figure 4.45: Calibration curve of the relative change in frequency shift according to different concentrations of <i>E. coli</i> O157:H7 DNA, display limit of detection (LOD).	141
Figure 4.46: Hybridization specificity demonstrated by the frequency shift of the complementary, one base mismatched and non-complementary DNA sequences.	142
Figure A1: Resonant frequency shift of 12 µm pitch size device after hybridization process with 1µM concentration complementary target.	168
Figure A2: Resonant frequency shift of 12 µm pitch size device after hybridization process with 1nM concentration complementary target.	168
Figure A3: Resonant frequency shift of 12 µm pitch size device after hybridization process with 1pM concentration complementary target.	169
Figure A4: Resonant frequency shift of 12 µm pitch size device after hybridization process with 1fM concentration complementary target.	169
Figure A5: Resonant frequency shift of 12 $\mu$ m pitch size device after hybridization process with 1 $\mu$ M concentration mismatched target.	170
Figure A6: Resonant frequency shift of 12 μm pitch size device after hybridization process with 1μM concentration non-complementary target	. 170
OTHISITE	

### LIST OF TABLES

NO	PAGE
Table 2.1: Comparison of the various types acoustic based sensor medium operation and sensitivity.	33
Table 2.2: Comparison of strip width for identical pitch size of threecommon IDTsconfigurations.	49
Table 2.3: Common surface acoustic wave piezoelectric substrates properties.	52
Table 2.4: Commonly used metals in IDT and their properties (Cardarelli, F., 2008).	53
Table 2.5: List of examples of salinization surface modification on $SiO_2$ covered devices and target analytes.	59
Table 3.1: IDT design parameters	64
Table 3.2: The material properties for $64^{0}$ YX LiNbO <sub>3</sub>	65
Table 3.3: Optimum Setting Parameters for Photolithography Process.	72
Table 3.4: Design data for $64^{0}$ YX LiNbO <sub>3</sub> piezoelectric substrate (aluminum metallization, with metallization ratio, $\eta$ =0.5).	75
Table 3.5: Experimental design matrix for IDT parameters sensitivity study.	77
Table 4.1: Summary of the simulation resonant frequencies of all the devices.	92
Table 4.2: Error fabrication for different pitch sizes IDT metal strips.	101
Table 4.3: Statistical analysis of different IDT pitch size fabrication.	109
Table 4.4: Comparison of resonant frequencies of fabricated pitch sizes to calculated shifted resonant frequencies caused by aluminum metallizatio	n. 110
Table 4.5: Experimental design matrix for IDT parameters sensitivity study wiresponses.	th 112
Table 4.6: Analysis of ANOVA for response surface linear model for temperate effect.	ture 113

Table 4.7: Analysis of ANOVA for response surface linear model for ma	ass loading
effect.	113

othis tem is protected by original copyright

Table 4.8: Previous acoustic wave-based biosensor for E. coli O157:H7 detection. 143

### LIST OF ABBREVIATIONS

- AFM Atomic force microscope
- **ANFIS** Adaptive neuro-fuzzy inference system
- ANN Artificial neural network
- ANOVA Analysis of variance
- APCVD Atmospheric pressure chemical vapor deposition original copyright
- APMS 3-aldehydepropyltrimethoxysilane
- APTES (3-Aminopropyl)triethoxysilane
- BAW Bulk acoustic wave
- cfu Colony-forming unit
- COM Coupling-of-modes
- CVD Chemical vapor deposition
- DNA Deoxyribonucleic acid
- Design of experiments DOE
- Enteroaggregative E. coli EAEC
- E.coli Escherichia coli
- EDX -ray Spectrometry
- EHEC Enterohemorrhagic E. coli
- Enteroinvasive E. coli EIEC
- **ELISA** enzyme-linked immunosorbent assay
- EPEC Enteropathogenic E. coli
- ETEC Enterotoxigenic E. coli
- **FBAR** Film bulk acoustic resonator
- **FEM** Finite element method
- FESEM Field emission scanning electron microscope
- FPW Flexural plate wave

FTIR	Fourier transform infrared spectroscopy
G6PDH	Glucose-6-phosphate dehydrogenase
Не	Helium
HPM	High-power microscopy
IANFIS	Improved adaptive neuro-fuzzy inference system
IC	Integrated circuit
IDT	Interdigital transducer
LPCVD	low pressure chemical vapor deposition
LiNbO3	Lithium niobate
LW	Love wave
MPTMS	3-mercaptopropyltrimethoxysilane
$N_2O$	Nitrous oxide
O <sub>2</sub>	Oxygen gas
OFAT	One factor at a time
ОН	Hydroxyl group
PBS	Phosphate buffer saline
PCR	Polymerase chain reaction
PECVD	Plasma enhanced chemical
PMMA	Polymethylmethacrylate
PNA	Peptide nucleic acid
PSA	Prostate specific antigens
PVD	Physical vapor deposition
QCM	Quartz crystal microbalance
RF	Radio frequency
RSAW	"Rayleigh-type" surface acoustic waves
RSD	Relative standard deviation
RSM	Response surface methodology

- SAW Surface acoustic wave
- SEM Scanning electron microscope
- SH-APM Shear horizontal acoustic plate mode
- SHSAW Shear horizontal surface acoustic wave
- SiO<sub>2</sub> Silicon oxide
- SiH<sub>4</sub> Silane
- SPR Surface plasmon resonance
- Surface skimming bulk wave **SSBW**

- copyright rave ficient of resonant from the theorem of theorem of theorem of the theorem of theorem of theorem of theore Temperature coefficient of resonant frequency

### LIST OF SYMBOLS

MHz	Mega hertz
cm	Centimeter
g	Gram
S <sub>m</sub>	Mass sensitivity
ρ	Substrate density
d	Substrate thickness
$K(\alpha)$	factor depending on the Poisson ratio
λ	wavelength
$A_0$	Asymmetric zero-order
$S_0$	Symmetric zero-order
h	Thickness of the wave guide film
hv	Photon energy
Hz	Hertz
R	Photolithography resolution
K <sub>1</sub>	Photolithography system constant
NA	Numerical aperture
mm	milimeter
[T]	Vector stress
[C]	Vector elastic stiffness coefficient
[S]	Vector strain
nm	nanometer
[E]	Vector electric field intensity
rpm	rounds per minute
[D]	Vector electrical displacement density

[3]	Vector permittivity
ü	Particle acceleration
F	Mechanical force acting on the substrate
φ	Electric potential
u	Mechanical displacement
Ω	Ohm
°C	Degree Celsius
μm	micrometer
Å	Angstrom
[a]	Rotation matrx
[M]	Transformation matrix
fo	Resonant frequency
v	Wave propagation velocity
pI	Periodicity
H(f)	Transfer function
K <sup>2</sup>	Electromechanical coupling coefficient
V <sub>out</sub>	Output signal voltage
V <sub>in</sub>	Input signal voltage
$C_s$	Capacitance for a strip pair per unit length
f O	Frequency
Ν	Number of strip pairs
W	Acoustic aperture
L	Delay line
kPa	Kilo pascal
ОН	Hydroxyl group
Si-O-Si	Silicon-oxygen

- $\mathbf{f}_{a}$ Average shifted resonant frequency
- Self-coupling coefficient k<sub>11</sub>
- Wave vector at resonant frequency  $k_0$
- Average shifted velocity  $v_a$
- $T_0$ Room temperature
- Δm Mass added
- $\Delta f$
- A
- μ
- Ø

othis tem is protected by original copyright

### Pembangunan Shear Horizontal Surface Acoustic Wave Dengan Silicon Dioxide Nanopartikel Pandu Gelombang Pengesan Untuk Pengesanan Escherichia Coli O157: H7

#### ABSTRAK

Escherichia coli (E.coli) O157: H7, iaitu sejenis strain berbahaya di antara 225 serotipe yang unik bagi E.coli. Beberapa sel bakteria ini dapat menyebabkan anak-anak muda berada dalam keadaan yang serius. Terdapat lebih daripada 1 cfu E.coli O157: H7 dalam 25 g makanan, telah dianggap sebagai tahap yang berbahaya. Tujuan penyelidikan ini adalah untuk membangunkan pengesan nanostruktur pandu gelombang (SHSAW) untuk mengesan E.coli O157: H7. Interdigital transducer (IDT) adalah peranti utama dalam pengesan SHSAW. Ia menentukan kekerapan salunan and kepekaan pengesan. Pada umumnya, lebih tinggi kekerapan salunan, pengesan lebih peka, dimana lebar IDT mesti dibuat untuk sub mikrometer. Ini akan melibatkan proses yang rumit dan kos tinggi. Walau bagaimanapun, beberapa laporan menyatakan bahawa rekabentuk IDT seperti bilangan elektrob penghantaran dan penerimaan, aperture akustik dan panjang kelewatan talian boleh meningkatkan kepekaan pengesan SHSAW. Dengan itu, simulasi COMSOL Multiphysics telah digunakan dalam penyelidikan ini dan hasilnya didapati aperture akustik dan panjang kelewatan talian boleh meningkatkan kepekaan pengesan. Kajian ini diteruskan dengan pembangunan dan penilaian fabrikasi peranti SHSAW dengan menggunakan proses litografi konvensional yang ditambahbaik. Hasil kajian menunjukkan peranti dapat difabrikasi di dalam makmal dengan dimensi peranti yang tepat (kurang daripada 1%, (RSD)) dan tepat (ralat kurang daripada 4% daripada pengiraan teori) dan boleh disambung untuk eksperimen mengkaji kepekaan IDT terhadap beban mass. Dari RSM, IDT saiz nada 12 µm dengan saiz bukaan 0.72 mm dan panjang kelewatan talian 2.1mm dengan purata frekuensi resonansi 385.1607 MHz dikenal pasti sebagai parameter yang paling optimum untuk mencapai kepekaan pengesan yang maksimum. Oleh itu, parameter IDT optimum terbukti lagi oleh eksperimen vang dapat mempengaruhi kepekaan beban mass. Kepekaan peranti bersaiz nada (12) µm dipertingkatkan lagi dengan mendepositkan 130.5 nm lapisan nipis nanostruktur SiO<sub>2</sub> dengan saiz zarah kurang daripada 70 nm. Nanostruktur ini bertindak sebagai pandu gelombang serta pengubahsuaian permukaan fizikal pengesan sebelum penetapan biomolekul. Satu urutan DNA tertentu daripada E. coli O157: H7 yang mempunyai 22 mers diguna sebagai ssDNA dengan hujungnya terdapat kumpulan amina yang ditetapkan pada kawasan lapisan nipis melalui tindakbalas kimia [(CHO-(CH<sub>2</sub>)<sub>3</sub>-CHO) dan (APTES; NH<sub>2</sub>-(CH<sub>2</sub>)<sub>3</sub>-Si(OC<sub>2</sub>H<sub>5</sub>)<sub>3</sub>]. Penderia yang prestasi tinggi ditunjukan degan mengesan sasaran oligonucleotide tertentu dengan kepekaan 0,6439 nM / 0.1 kHz dan had pengesanan serendah 1.8 femto-molar (1.8 x 10-15 M). Prestasinya terus dinilai oleh analisis kekhususan dengan menggunakan satu urutan oligonucleotide yang satu tidak sepadan dan komplementari.

### Development of Shear Horizontal Surface Acoustic Wave with Silicon Dioxide Nanoparticles Waveguide Sensor for *Escherichia Coli* O157:H7 Detection

#### ABSTRACT

Escherichia coli O157:H7 (E.coli O157:H7), a dangerous strain among 225 E. coli unique serotypes. A few cells of this bacterium are able to cause young children to be most vulnerable to serious complications. The presence of higher than 1 cfu E .coli O157:H7 in 25 g of food has been considered as a dangerous level. Thus, highly sensitive sensor is needed for this. The aim of this research work is to develop nanostructure waveguide shear horizontal surface acoustic wave (SHSAW) sensor for the detection of E.coli O157:H7. The interdigital transducer (IDT) is the heart of SHSAW sensor. It determines the resonant frequency and the sensitivity of the sensor. In generally, the higher the resonant frequency, the higher sensitive the sensor will be, the width of IDT has to fabricated to sub micrometer. These involve more expensive cost and complicated methods. However, few reports mentioned IDT design parameters such number of transmission and receiving electrode fingers, electrode length or acoustic aperture and length of delay line or propagation path, can increase the SHSAW sensor sensitivity. Herein, COMSOL Multiphysics simulations were implemented for this investigation, the delay line length and aperture sizes are found that can increase the mass loading sensitivity. The research was continued by the development and evaluation of fabrication SHSAW device by using the improved conventional lithography process was conducted. The results show that the dimension of devices were precisely(less than 1%, relative standard deviation (RSD)) and accurately (less than 4% error from theoretical calculation) fabricated in laboratory for experimentally study on the effects of IDT parameters toward mass loading sensitivity. From the response surface methodology, 12 µm pitch sizes IDT with 0.72 mm aperture size, 2.1 mm delay line length and 385.1607 MHz average resonant frequency were identified as the most optimum parameters to achieve highest sensitive of devices. Thus, these optimum IDT parameters were further proven by real experiments that able to affect the mass loading sensitivity. The 12 pitch size device was further enhanced by depositing 130.5 nm thin layer of SiO<sub>2</sub> nanostructures with particle size lesser than 70 nm. The nanostructures act both as a waveguide as well as a physical surface modification of the sensor prior to biomolecular immobilization. A specific DNA sequence from E. coli O157:H7 having 22 mers as an amine-terminated probe ssDNA was immobilized on the thin film sensing area through chemical functionalization [(CHO-(CH<sub>2</sub>)<sub>3</sub>-CHO) and (APTES; NH<sub>2</sub>-(CH<sub>2</sub>)<sub>3</sub>-Si(OC<sub>2</sub>H<sub>5</sub>)<sub>3</sub>]. The high-performance of sensor was shown with the specific oligonucleotide target and attained the sensitivity of 0.6439 nM/ 0.1 kHz and detection limit was down to 1.8 femto-molar (1.8 x 10<sup>-15</sup> M). Further evidence was provided by specificity analysis using single mismatched and complementary oligonucleotide sequences.

#### **CHAPTER 1**

#### INTRODUCTION

#### 1.1 Introduction

In 1885, the bacteriologist Theodor Escherich discovered the existence of Escherichia coli (E. coli) bacteria in the human colon (Feng et al., 2002). Today, many E. coli strains are known to exist in the digestive tract of humans and animals. Many of these are harmless and can act as normal microbiotas with mutual benefits for the bacteria and the host (Drasar & Hill, 1974). However, some strains that have undergone evolutionary changes which possess virulence factors to be pathogens (Lim, Yoon, & Hovde, 2010). These pathogenic *E. coli* can be divided into at least six categories based on their pathogenic mechanisms. The five most well known categories are the enteropathogenic E. coli (EPEC), enteroaggregative E. coli (EAEC), enteroinvasive E. coli (EIEC), enterotoxigenic E. coli (ETEC) and enterohemorrhagic E. coli (EHEC) (Nataro & Kaper, 1998). The EHEC produce exotoxins known as verotoxins (also termed Shiga-like toxins) that cause several diseases, from mild diarrhea to potential fatal hemorrhagic thrombotic colitis, hemolytic uremic syndrome, and thrombocytopenic purpura (Goswami, Chen, Xiaoli, Eaton, & Dudley, 2015; Rahal, Kazzi, Nassar, & Matar, 2014; Wong et al., 2012).

One of the most dangerous EHEC serotypes, *E. coli* O157:H7, was first recognized in 1982 as a human pathogen associated with outbreaks of bloody diarrhea in Oregon and Michigan, U.S.A. (Wells et al., 1983). Since then, *E. coli* O157:H7

outbreaks have been reported in at least 30 countries on six continents ((Dundas et al., 2001; Michino et al., 1999; Doyle & Buchanan, 2012) with young children and the aged being most vulnerable to serious complications (Griffin & Tauxe, 1991). In Malaysia alone, there have been 62 cases of food poisoning by *E. coli* O157:H7 in 2008 and 36 cases in 2009 (Soon, Singh, & Baines, 2011). The actual number of cases, however, is likely to be higher due to a lack of foodborne disease intensive monitoring and surveillance in Malaysia (Soon, et al., 2011). Estimated of 73,480 illnesses, 2,168 hospitalizations, and 61 deaths due to the infections by *E. coli* O157:H7 annually in the United States has been reported by Centers for Disease Control and Prevention, Atlanta, Georgia, USA (Mead et al., 1999). In the U.S.A, the Center for Disease Control and Prevention in Atlanta, Georgia, estimates that there are 73 480 cases of *E. coli* O157:H7 each year in the U.S.A, resulting in 2168 hospitalizations and 61 deaths (Mead et al., 1999; C.-T. J. Lin, Jensen, & Yen, 2005), costing over US\$400 million per annum (Frenzen, Drake, Angulo, & Group, 2005).

The *E. coli* O157:H7 bacteria can easily be transmitted through untreated water supply, undercooked or raw meat, milk, fruits, vegetables, food and shared use of facilities (Olsen et al., 2002; Rahal, et al., 2014; Varma et al., 2003; Wendel et al., 2009). While conventional bacterial detection methods and microbiological techniques (pre-enrichment, selective enrichment, biochemical screening and serological confirmation) can be used to detect and identify outbreaks of this bacteria, this process is labour intensive and time consuming (18-24 hours or longer) (Hobson, Tothill, & Turner, 1996; Tietjen & Fung, 1995). In addition, there are more than 1000 *E. coli* serotypes and it is very difficult to distinguish *E. coli* O157:H7 from other close serotypes (Ørskov & Ørskov, 1992). Biosensors with higher sensitivity, and rapid and accurate detection of *E. coli* O157:H7 would greatly improve food security.