DESIGN OF A PORTABLE CONTINUOUS SYSTOLIC BLOOD PRESSURE MONITORING KIT WITH BUILT-IN LOW AND HIGH

BLOOD PRESSURE EARLY WARNINGS

RNI. COTIOSINAL COTIOSINAL COTIOSINAL MUHAMAD KHAIRUL BIN ALI HASSAN

orthis item is pr **UNIVERSITI MALAYSIA PERLIS**



DESIGN OF A PORTABLE CONTINUOUS SYSTOLIC BLOOD PRESSURE MONITORING KIT WITH BUILT-IN LOW AND HIGH BLOOD PRESSURE EARLY WARNINGS

MUHAMAD KHAIRUL BIN ALI HASSAN (0630610102)

by

Á thesis submitted In fulfilment of the requirements for the degree of Master of Science (Mechatronic Engineering)

School of Mechatronic Engineering UNIVERSITI MALAYSIA PERLIS

ACKNOWLEDGEMENTS

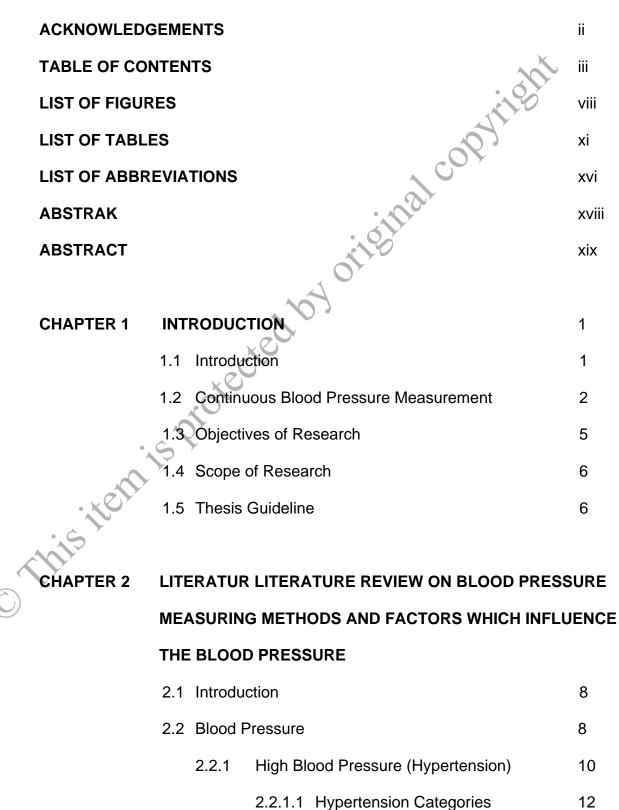
Firstly, I would like to acknowledge that this project is supported under eScience Fund Grand, 9005-00024, entitle, "Design of a portable continuous systolic blood monitoring kit with built-in low and high blood pressure early warnings". My special thank to my supervisor Prof. Dr. Mohd Yusoff Mashor for his guidance, support and encouragement. Then, I would like to express my sincere gratitude to my co-supervisors, Assoc. Prof. Abd Rahman Mohd Saad (School of Computer Engineering,) and Dr. Mohd Sapawi Mohamed (Department of Cardiology, Hospital Universiti Sains Malaysia (HUSM)) for their guidance, support, comments and discussions.

I would also like to thank the staff of HUSM for their cooperation in providing guidance and support during data collection. My appreciation also goes to the Biomedical Lab members for providing me with the necessary equipment to help in this research work.

Big thanks go to my parents, wife and family for their endless advice, love and prayers. Special thanks also go to my friends, who have helped me one way or another to remove the obstacles and difficulties faced in this research. Last but not least, I would like to thank to Universiti Malaysia Perlis for its financial assistance through the Skim Latihan Akademi Bumiputera (SLAB). Without it, this research work would never have commenced.

ii





PAGE

			2.2.1.2 High Blood Pressure in Children	13
		2.2.2	Blood Pressure Range and Action Taken	14
		2.2.3	Low Blood Pressure	16
			2.2.1.1 Symptom and Signs Low Blood	
			Pressure	16
			2.2.1.2 Diagnosis and Evaluation of Low	
			Blood Pressure	17
			in a	
	2.3	The He	art and Electrocardiogram	18
		2.3.1	ECG Morphology	20
		2.3.2	History of ECG	22
		2.3.3	ECG and Heart Rate	23
	2.4	Relation	n between Heart Rate and Blood Pressure	25
٥	2.5	Pulse V	Vave Transit Time (PWTT)	28
	2.6	Noninva	asive Blood Pressure Measurement Methods	30
·KOL	2.7	Summa	ıry	32
ands -				
CHAPTER 3	SYS	STEM DI	EVELOPMENT	
	3.1	Introdu	ction	34
	3.2	Block D	Diagram of Portable Blood	
		Pressu	re Monitoring Kit	34
	3.3	8051 D	evelopment Board	36
	3.4	Input/O	utput Devices	37
		3.4.1	Keypad	37

	3.4.2	Liquid Crystal Display	38
	3.4.3	Serial EEPROM	39
	3.4.4	Switch	40
	3.4.5	Input Sensor	40
	3.4.6	ECG Amplifier	42
		3.4.6.1 Instrumentation Amplifier	44
		3.4.6.2 Low Pass Filter	45
		3.4.6.3 High Pass Filter	47
	3.4.7	Warning System	48
3.5	Memory		48
3.6	Interfac	ing Part	49
	3.6.1	MAX232	51
	3.6.2	DB-9 Serial Port Connector	51
3.7	Power	Supply Circuit	52
3.8	Summa	ıry	53
· KON			
CHAPTER 4 RES	SULT AN	ID DATA ANALYSIS	
4.1	Introduc	ction	54
4.2	Continu	ous Systolic Blood Pressure Monitoring Kit	54
4.3	Continu	ous Monitoring of Systolic Blood Pressure	
	Based	on PWTT	55
	4.3.1	Data Collection of Pulse Wave Transit Time	
		(PWTT)	57
	4.3.2	Result and Discussion based on Linear	

		Regression Model	58
	4.3.3	Result and Discussion based on	
		Non-Linear Regression Model	67
	4.3.4	Result and Discussion based on Neural	
		Network Model	75
4.4	Continu	ous Monitoring of Systolic Blood Pressure	
	Based	on Heart Rate	79
	4.4.1	Data Collection of Heart Rate (HR)	81
	4.4.2	Result and Discussion based on Linear	
)	Regression Model	82
	4.4.3	Result and Discussion based on Non-Linear	
~	sto-	Regression Model	91
	4.4.4	Result and Discussion based on Neural	
teli		Network Model	100
4.5	Compa	rison between Continuous Measuring Blood	
	Pressur	e Based on PWTT and Heart Rate	104
4.6	Conclus	sion	105

CHAPTER 5 VALIDATION OF A PROPOSED PORTABLE BP MONITORING KIT

Introduction	107
	Introduction

5.	2 Continuous Systolic Blood Pressure Monitoring Kit	
	Based on Heart Rate	107
5.	3 Validation Process	112
5.	4 Result and discussion	112
5.	5 Conclusion	123
CHAPTER 6 CO	ONCLUSION Conclusion	
6.7	Conclusion	125
6.2	2 Suggestions for Future Work	128
REFERENCES	cted by	129
APPENDIX A Co	ntinuous BP Monitoring Kit Testing	135
APPENDIX B	aluation Questionnaire	165
APPENDIX C PI	N Descriptions	192
LIST OF PUBLICA	TIONS	198
\bigcirc		

LIST OF FIGURES

			PAGE
	Figure 2.1	Label of ECG waveform	19
	Figure 2.2	Period for P, Q, R, S and T segment	20
	Figure 2.3	An illustration of the definition of Pulse Wave Transit	
		Time (PWTT)	28
	Figure 3.1	Overall Block Diagram of Portable Systolic Blood	
		Pressure Monitoring Kit	35
	Figure 3.2	Schematic Diagram of the Input/Output Part	35
	Figure 3.3	8051 Development Board	36
	Figure 3.4	Internal structures of a 4 x 3 keypad and its connection	
	• Ĉ	to the 8051 microcontroller	38
	Figure 3.5	Physical structure of the LCD part	39
	Figure 3.6	Schematic diagram of ECG Amplifier and Filter	41
	Figure 3.7	ECG signal with noises	43
	Figure 3.8	Three-op-amp Differential Amplifier	44
Ŋ	Figure 3.9	Connection Diagram of AD624	45
	Figure 3.10	Basic Second Order Low-Pass Filter	45
	Figure 3.11	Low-Pass Sallen-Key Circuit	46
	Figure 3.12	Basic High-Pass Filter	47

	Figure 3.13	High-Pass Sallen-Key Circuit	48
	Figure 3.14	The flow of data from the computer to the RAM and	
		then to EEPROM	50
	Figure 3.15	Schematic Diagram of the Interfacing part	50
	Figure 3.16	DB-9 Connector	51
	Figure 3.17	Power supply circuit	52
	Figure 4.1	Block diagram of process flow of development of	
		regression model	56
	Figure 4.2	Samples of SBP versus PWTT for Subject 1	58
	Figure 4.3	Samples of SBP versus PWTT for Subject 2	58
	Figure 4.4	Samples of SBP versus PWTT for Subject 3	59
	Figure 4.5	Test data of SBP versus PWTT for Subject 1	61
	Figure 4.6	Test data of SBP versus PWTT for Subject 2	61
	Figure 4.7	Test data of SBP versus PWTT for Subject 3	61
	Figure 4.8	Test data SBP vs. PWTT using non-linear model for	
		Subject 1	67
	Figure 4.9	Test data SBP vs. PWTT using non-linear model for	
\bigcirc		Subject 2	68
	Figure 4.10	Test data SBP vs. PWTT using non-linear model for	
		Subject 3	68
	Figure 4.11	Architecture of neural network	76
	Figure 4.12	Result of mean square error (MSE) against hidden	76

neurons

	Figure 4.13	An illustration of the definition of R-R interval	80
	Figure 4.14	Block diagram of process flow of regression analysis	81
	Figure 4.15	Data SBP vs. HR of Subject 1	83
	Figure 4.16	Data SBP vs. HR of Subject 2	83
	Figure 4.17	Data SBP vs. HR of Subject 3	83
	Figure 4.18	Test data SBP vs. HR using non-linear model for	
		Subject 1	92
	Figure 4.19	Test data SBP vs. HR using non-linear model for	
		Subject 2	92
	Figure 4.20	Test data SBP vs. HR using non-linear model for	
		Subject 3	92
	Figure 4.21	Result of Mean Square Error (MSE) against Hidden	
	•	Neurons	100
	Figure 5.1	Flow of the system operation	108
	Figure 5.2	A portable blood pressure monitoring kit	110
	Figure 5.3	A portable BP monitoring kit with normal systolic blood	110
\bigcirc		pressure value	
	Figure 5.4	A portable BP monitoring kit with high systolic blood	111
		pressure value	
	Figure 5.5	A portable BP monitoring kit with low systolic blood	111
		pressure value	

LIST OF TABLES

Table 2.1	Categories of Blood Pressure and Action Taken	15
Table 2.2	Target heart rate during exercise (AAMI, 1993)	25
Table 3.1	Descriptions of LCD	39
Table 3.2	Memory Addressing System	49
Table 3.3	Description of DB-9 connector pins	52
Table 4.1	Original and new linear regression models for the	
	subjects	60
Table 4.2	The comparison of SBP data of Subject 1 after applying	
	new method	62
Table 4.3	The comparison of SBP data of Subject 2 after applying	
	new method	63
Table 4.4	The comparison of SBP data of Subject 3 after applying	
nis	new method	64
Table 4.5	(a) The summary of all original linear regression models	
	(Based on PWTT)	65
	(b) The summary of all new linear regression models	
	(Based on PWTT)	
		66
Table 4.6	Original and new non-linear regression models for each	68

subject

Table 4.7	The comparison of SBP data of Subject 1 after applying	
	new non-linear regression models	70
Table 4.8	The comparison of SBP data of Subject 2 after applying	
	new non-linear regression models	71
Table 4.9	The comparison of SBP data of Subject 3 after applying	
	new non-linear regression models	72
Table 4.10	(a) The summary of all original non-linear regression	
	models (Based on PWTT)	73
	(b) The summary of all new non-linear regression	
	models (Based on PWTT)	74
Table 4.11	Training PWTT and BP data for Neural Network	77
Table 4.12	Testing PWTT and BP data for Neural Network	78
Table 4.13	Regression model analysis using heart rate for each	
. YOL	individual SBP	84
Table 4.14	Original and new linear regression models for each	
	subject	85
Table 4.15	The comparison of SBP data of Subject 1 after applying	
	new linear regression models	86
Table 4.16	The comparison of SBP data of Subject 1 after applying	
	new linear regression models	87

Table 4.17	The comparison of SBP data of Subject 1 after applying	
	new linear regression models	88
Table 4.18	(a) The summary of all original linear regression models	
	(Based on Heart Rate)	89
	(b) The summary of all new linear regression models	
	(Based on Heart Rate)	90
Table 4.19	Original and new non-linear regression based on HR	
	models for each subject	93
Table 4.20	The comparison of SBP data of Subject 1 after applying	
	non-linear model	94
Table 4.21	The comparison of SBP data of Subject 2 after applying	
	non-linear model	95
Table 4.22	The comparison of SBP data of Subject 3 after applying	
	non-linear model	96
Table 4.23	The comparison of SBP of Subject 4 after applying non-	
····	linear model	97
Table 4.24	(a) The summary of all original regression models	
	(Based on Heart Rate)	98
	(b) The summary of all new regression models (Based	
	on Heart Rate)	99
Table 4.25	Training HR and BP data for Neural Network	101
Table 4.26	Testing HR and BP data for Neural Network	102

Table 4.27	Comparison the technique for measuring systolic blood	
	pressure	104
Table 5.1	The Normal Systolic Blood Pressure data of Subject 1	113
Table 5.2	The Normal Systolic Blood Pressure data of Subject 2	114
Table 5.3	The Normal Systolic Blood Pressure data of Subject 3	115
Table 5.4	The Low Systolic Blood Pressure data of Subject 4	116
Table 5.5	The Low Systolic Blood Pressure data of Subject 5	117
Table 5.6	The Low Systolic Blood Pressure data of Subject 6	118
Table 5.7	The High Systolic Blood Pressure data of Subject 7	119
Table 5.8	The High Systolic Blood Pressure data of Subject 8	120
Table 5.9	The High Systolic Blood Pressure data of Subject 9	121
Table 5.10	The summary of all data subjects	123

LIST OF ABBREVIATIONS

- AAMI Association Advancement of Medical Instrumentation
- ABP Arterial Blood Pressure
- AgCI Argentums Chloride
- BP Blood Pressure
- bpm beats per minute
- DBP Diastolic Plood Pressure
- ECG Electrocardiograph
- EEPROM Electrically Erasable Programmable Read Only Memory

121 copyright

- EMFi Electromechanical film
- EMG Electromyogram
- Gnd Ground

I/O

LCD

LED

LM

- HR Heart Rate
 - 🐪 Input/Output
 - Liquid Crystal Display
 - Light Emitting Diode
 - Levenberg-Marquardt
- MHR Maximum Heart Rate
- mmHg millimeters of mercury
- MOE Mean of Error
- MSE Mean Square Error
- NN Neural Network
- PPG Photoplethysmographic

- **PWTT Pulse Wave Transit Time**
- ROM Read Only Memory
- onthis teen is protected by original convited the

REKABENTUK ALAT PEMANTAUAN TEKANAN DARAH SISTOLIK BERTERUSAN MUDAH ALIH DENGAN SISTEM AMARAN AWAL BAGI TEKANAN DARAH RENDAH DAN TINGGI

ABSTRAK

Kira-kira satu daripada tiga orang dewasa di Amerika Syarikat mempunyai tekanan darah tinggi tetapi tekanan darah tinggi sahaja biasanya tidak mempunyai tanda-tanda. Lazimnya, hipertensi bagi penduduk Malaysia yang berumur 31 tahun keatas adalah lebih daripada 42.6%. Sebahagian besar kes (64%) di negara ini masih tidak dikenalpasti. Hanya 26% daripada pesakit Malaysia mencapai tekanan darah terkawal (<140/90 mmHg). Pada masa kini, ramai orang mempunyai tekanan darah tinggi selama bertahun-tahun tanpa mengetahuinya. Tekanan darah tinggi tidak terkawal boleh menyebabkan strok, serangan jantung, kegagalan jantung atau kegagalan buah pinggang. Perkara inilah yang menyebabkan tekanan darah tinggi dipanggil 'silent killer'. Hanya satu cara untuk mengenalpasti tekanan darah anda iaitu dengan mengukur tekanan darah. Tekanan darah kebiasaannya diukur dengan menggunakan peranti yang dipanggil sphygmomanometer, stetoskop dan manset tekanan darah. Kebanyakkan teknik yang digunakan untuk mengukur tekanan darah secara automatik atau manual adalah tidak bersesuaian untuk mengukur tekanan darah secara berterusan. Objektif kajian ini adalah untuk membangunkan satu alat mudah alih yang boleh mengukur tekanan darah secara berterusan dengan menggunakan sensor electrocardiography (ECG) dan sensor denyut. Dua kaedah telah digunakan untuk mengukur tekanan darah secara berterusan. Kaedah pertama yang telah digunakan untuk mengukur tekanan darah secara berterusan adalah berdasarkan kadar degupan jantung (HR) dan kaedah kedua adalah berdasarkan 'Pulse Wave Transit Time' (PWTT). Kedua-dua kaedah ini dibahagikan kepada dua teknik yang berbeza bagi mengukur tekanan darah sistolik. Teknik-teknik yang telah digunakan untuk merekabentuk hubungan diantara data PWTT/HR dan tekanan darah sistolik adalah model regresi lurus, model regresi tidak lurus dan model rangkaian neural. Model rangkain neural memberi nilai terkecil bagi purata ralat dan ralat sisihan piawai untuk pengukuran tekanan darah berdasarkan PWTT atau HR. Ralat-ralat ini adalah boleh diterima dan agak kecil berbanding ketepatan piawai, yang sepatutnya mempunyai nilai purata ralat 6 mmHg dan ralat sisihan piawai ±10mmHg. Subjek-subjek yang telah terlibat dalam pengujian alat pemantauan tekanan darah ini adalah subjek tekanan darah normal, subjek tekanan darah rendah dan subjek tekanan darah tinggi. Kesemua data telah diambil dalam masa 5 minit untuk setiap subjek dan hasil ujian telah dipantau oleh pakar jantung/doktor atau jururawat. Ketepatan data daripada sistem pemantaun BP berterusan telah disahkan menggunakan sphygmomanometer. Hasil ujian menunjukkan alat sistem BP yang telah dibangunkan ini adalah sesuai digunakan untuk mengukur atau memantau tekanan darah sistolik secara berterusan. Sistem amaran telah dibangunkan di dalam alat pemantaun BP ini. Sistem amaran berfungsi berdasarkan nilai tekanan darah dan tren naik turun nilai tekanan darah sistolik. Sistem amaran ditunjukkan dalam bentuk penggera. Penggera akan aktif apabila nilai tekanan darah sistolik lebih daripada 140mmHq (Tekanan Darah Tinggi) atau kurang daripada 100mmHg (Tekanan Darah Rendah) atau jika tren tekanan darah sistolik meningkat atau menurun lebih daripada 5mmHg untuk setiap 30 saat.

DESIGN OF A PORTABLE CONTINUOUS SYSTOLIC BLOOD PRESSURE MONITORING KIT WITH BUILT-IN LOW AND HIGH BLOOD PRESSURE EARLY WARNINGS

ABSTRACT

About one in three adults in the United States have high blood pressure but high blood pressure itself usually has no symptoms. The prevalence of hypertension in Malaysians aged 30 years and above was 42.6%. The majority of cases (64%) in this country remain undiagnosed. Only 26% of Malaysian patients achieved blood pressure control (<140/90 mmHg). Now days, many people have high blood pressure for years without knowing it. Uncontrolled high blood pressure can lead to stroke, heart attack, heart failure or kidney failure. This is why high blood pressure is often called the "silent killer." The only way to tell if you have high blood pressure is to have your blood pressure checked. Blood pressure is often measured using a device called a sphygmomanometer, a stethoscope and a blood pressure cuff. Almost all the existing manual or automatic measuring techniques of blood pressure are based on this principle, which is not convenient for continuous monitoring of blood pressure. The objective of this study is to develop a portable continuous blood pressure monitoring system using an electrocardiography (ECG) sensor and a pulse sensor. Two methods were used to measure blood pressure continuously. The first method measures blood pressure continuously based on Heart Rate (HR) and the second method is based on Pulse Wave Transit Time (PWTT). Both methods were separately implemented for different techniques to measure systolic blood pressure (SBP). The techniques that were used to model the relationship between the PWTT or HR data to systolic blood pressure are linear regression model, non-linear regression model and neural network model. Neural network model gave the smallest value of mean of error and standard deviation of error for measuring blood pressure based on PWTT or HR. These errors are acceptable and relatively small compared to the standard accuracy, which should have a minimum mean of error value of 6 mmHg with a standard deviation of error of ± 10 mmHg. The subjects that were involved in portable BP monitoring kit testing are normal blood pressure subjects, low blood pressure subjects and high blood pressure subjects. All the data were taken about five minutes for each subject and the results were monitored by medical cardiologist/doctor or nurses. The accuracy of the SBP data from portable continuous BP monitoring kit was validated using sphygmomanometer. The results indicate that the developed portable BP system is adequate to be used for monitoring or measuring systolic blood pressure continuously. Warning system was developed in this portable BP monitoring kit. The warning system is generated based on blood pressure value and trend of increasing or decreasing of systolic blood pressure values. The warning is given in form of alarm. The alarm will be "on" when the systolic blood pressure value goes more than 140mmHg (High Blood Pressure) or less than 100mmHg (Low Blood Pressure) or if the SBP increasing or decreasing trend in more than 5mmHg for each 30 seconds.

CHAPTER 1

INTRODUCTION

1.1 Introduction

In fact, nearly one in three United State adults has high blood pressure, but because there are no symptoms, nearly one-third of these people do not know they have it (American Heart Association, 2008). The prevalence of hypertension in Malaysians aged 30 years and above was 42.6%. The majority of cases (64%) in the country remain undiagnosed. Only 26% of Malaysian patients achieved blood pressure control (<140/90 mmHg) (Ministry of Health, 2008). Now days, many people have high blood pressure for years without knowing it. Uncontrolled high blood pressure can lead to stroke, heart attack, heart failure or kidney failure. This is why high blood pressure is often called the "silent killer." The only way to tell if you have high blood pressure is to have your blood pressure (BP) checked.

Arterial blood pressure is most accurately measured invasively by placing a cannula into a blood vessel and connecting it to an electronic pressure transducer. This invasive technique is regularly employed in intensive care medicine, anesthesiology and for research purposes. However, it is associated (rarely) with complications such as thrombosis, infection, and bleeding.

The non-invasive auscultatory and oscillometric measurements are simpler and quicker, require less expertise in fitting, have no complications, and are less unpleasant and painful for the patient. In addition, the methods are less accurate and have small systematic differences in numerical results. These methods

actually measure the pressure of an inflated cuff at the points where it just occludes blood flow, and where it just permits unrestricted flow. These are the methods commonly used for routine examinations and monitoring. Nevertheless, the accuracy of these devices has not yet reached the necessary level, since only some of them are clinically validated and most have a questionable accuracy (O'Brien, 2001).

Two numbers are used to describe blood pressure, which are systolic blood pressure and diastolic blood pressure. Blood pressure is often measured using a device called a sphygmomanometer, a stethoscope, and a blood pressure cuff (Webster, 1998; Sola, 2007). The cuff is placed around the upper arm and filled with air. This tightening effect is used to stop the blood from flowing through the brachial artery of the arm. The stethoscope is placed over the artery in front of the elbow and the pressure in the cuff is slowly released. No sound is heard until the cuff pressure falls below the systolic pressure in the artery, at this point, a pulse is heard. As the cuff pressure continues to fall slowly, the pulse continues, first becoming louder, then dull and muffled. The cuff pressure at the point at which the first sounds are heard, is defined as the systolic blood pressure (SBP). The cuff pressure at the point at which the sounds stop, is defined as the diastolic blood pressure. A doctor would quote patients blood pressure as the value of the systolic pressure.

1.2 Continuous Blood Pressure Measurement

In recent years there has been increasing interest in wearable health monitoring devices, both in research and in industry. These devices are particularly

important to the world's increasingly aging population, whose health has to be assessed regularly or monitored continuously in daily life (Tr"oster, 2005). Blood pressure has been an important physiological parameter. However, no fully satisfactory ambulant sensor exists up to now for long-term and continuous monitoring (Hereyan, 2007; Berner, 2008). Those devices that utilized an occlusive cuff are not fully wearable and unobtrusive. Therefore, it is clear that new techniques for monitoring the blood pressure without the use of cuff are needed.

Teng and Zhang (2003) published the paper of Continuous and Noninvasive Estimation of Arterial Blood Pressure (ABP) using a Photoplethysmographic (PPG) Approach. Their study examines the relationships between arterial blood pressure and certain features of the photoplethysmographic signals obtained from I5 healthy subjects. Width of 1/2 pulse amplitude, width of 2/3 pulse amplitude, systolic upstroke time and diastolic time of the pulse were selected as features of the PPG signals. It was found that the diastolic time has higher correlation with systolic blood pressure and diastolic blood pressure than other features. The estimated results using diastolic time are better than the results using systolic upstroke time. The preliminary results indicate that it is possible to use the photoplethysmography only for cuffless and continuous estimation of arterial blood pressure.

Kerola et al. (1997) proposed a method to measure blood pressure continuously, which used an arm cuff with two electromechanical film (EMFi) sensors under it. The delay change between signals from these sensors was to be measured by the cross-correlation method. Later on, Sorvoja and Myllylä (2005) proposed a method, where an EMFi sensor is used to sense radial artery pulsations and a cuff is placed around the upper arm to occlude the brachial artery.

Blood pressure determination was based on either pulse amplitude change or pulse wave transit time (PWTT) change.

Teng & Zhang (2003) published a paper describing a method for noninvasive and cuffless blood pressure measurements on 15 young, healthy subjects. They used photoplethysmograph (PPG) sensor and electrocardiograph (ECG) sensor to measure blood pressure values. To provide reference measurements, they used an oscillometric BP-8800 device manufactured by Colin, Ltd. Measurements, taken at three different stages: rest, step-climbing exercise and recovery from the exercise, indicated the mean of error is (7.3 ± 0.2) mmHg for systolic and (4.4 ± 0.2) mmHg for diastolic blood pressure. A year later, Hung et al. (2004) reported a wireless measurement concept using Bluetooth for telecommunication from a PPG sensor to a mobile phone, PC or PDA device. The achieved mean of error is (8.6 ± 1.8) mmHg for systolic and (6.3 ± 0.5) mmHg for diastolic blood pressure. This study proved that the proposed technique (PWTT) is suitable for measuring blood pressure of healthy subjects.

Poon & Zhang (2005) extended the measurements to include the subjects aged 28 to 86 years, which included hypertensive subjects. These measurements were conducted over an average period of 6.4 weeks. They collected about one thousand pairs of systolic and diastolic blood pressure values. Reference results were provided by the average of results measured by a nurse using the auscultatory method and results obtained using two clinically approved automated blood pressure meters (BP-8800 Colin, Ltd and HEM-907, Omron, Ltd). Poon & Zhang reached the value of (9.8 \pm 1.6) mmHg for systolic and (6.6 \pm 1.9) mmHg for diastolic blood pressure. The results obtained in this study indicated that the value of diastolic blood pressure and systolic blood pressure are suitable for cuffless measuring blood pressure.

Berner (2008) designed CNAP[™] Monitor 500, it performs continuous noninvasive blood pressure monitoring. The unit can be used in conjunction with other monitoring systems or alone as a self contained, battery powered unit. CNAP[™] traces blood pressure changes through the patented CNAP[™] cuff at the fingers. However, until recently only invasive methods provided quality information to the clinician. CNAP[™] provides reliable blood pressure monitoring comparable to invasive techniques and adds valuable information about fluid responsiveness of the patient non-invasively.

1.3 Objectives of Research

The main objective of this study is to develop a portable continuous blood pressure monitoring kit with built-in low and high blood pressure early warnings. The specific objectives of this research are mentioned as below:

• To identify the parameters that are used to measure blood pressure.

To formulate and validate the mathematical models between the affecting parameters and systolic blood pressure.

- To develop a portable and low cost blood pressure monitoring kit based on the selected mathematical model.
- To develop the high and low blood pressure early warnings function. The warning system is generated based on blood pressure value and trend of increasing or decreasing of systolic blood pressure values.