

# COMPACT INGESTIBLE PLANAR INVERTED-F ANTENNA (PIFA) FOR BIOTELEMETRY SYSTEMS

# MUHAMMAD SOLIHIN BIN ZULKEFLI (1040910503)

A thesis submitted in fulfillment of the requirements for the degree of Doctor of Philosophy

# School of Electrical Systems Engineering UNIVERSITI MALAYSIA PERLIS

2015

# **UNIVERSITI MALAYSIA PERLIS**

	DECLARATION OF THESIS
Author's full name :	Muhammad Solihin bin Zulkefli
Date of birth :	21/09/1986
Title :	Compact Ingestible Planar Inverted-F Antenna (PIFA)
	for Biotelemetry Systems.
	2015
Academic Session :	2015
I hereby declare that the the at the library of UniMAP. Th	esis becomes the property of Universiti Malaysia Perlis (UniMAP) and to be placed is thesis is classified as :
	(Contains confidential information under the Official Secret Act 1972)*
	(Contains restricted information as specified by the organization where research was done)*
X OPEN ACCESS	I agree that my thesis is to be made immediately available as hard copy or on-line open access (full text)
I, the author, give permissi research or academic excha	on to the UniMAP to reproduce this thesis in whole or in part for the purpose of ange only (except during a period of years, if so requested above).
(h)	Certified by:
SIGNATUR	E SIGNATURE OF SUPERVISOR
860921-35- (NEW IC NO. / PAS	-5587 Assoc. Prof. Dr. Mohd Fareq bin Abd. Malek SPORT NO.) NAME OF SUPERVISOR
Date : 30/07/20	Date : 30/07/2015

**NOTES**: \* If the thesis is CONFIDENTIAL or RESTRICTED, please attach with the letter from the organization with period and reasons for confidentially or restriction.

# THESIS DECLARATION

o this item is protected by original copyright

#### ACKNOWLEDGEMENT

I am extremely grateful for the guidance and feedback I received throughout my research years from my supervisor Assoc. Prof. Dr. Mohd Fareq bin Abd Malek, from my co-supervisors, Prof. Dr. Syed Idris bin Syed Hassan, Assoc. Prof. Dr. Faizal bin Jamlos and my supervisor during attachment program at Lougborough University, United Kingdom, Dr. William G. Whittow for their knowledge sharing and constructive comments and suggestions. Their constant encouragement and support helped me significantly in my PhD journey.

I would like to acknowledge the Universiti Malaysia Perlis (UniMAP), Malaysia and the Ministry of Higher Education Malaysia for the financial support in the form of a scholarship throughout my PhD study. Special thanks are due to Masyarakat Melayu Loughborough (MML) for their valuable friendship and helps during my stay at Loughborough, United Kingdom.

Last but not least, I would like to express gratitude to my father Zulkefli bin Ahmad, my mother Nor Asikin binti Zakaria, my late grandfather Zakaria bin Awang, my grandmother Siti Sauyah binti Isa, my lovely wife Nurul Awanis binti Johan and my father and mother in-law, for their love, support and encouragement during my PhD journey. Without their consistent support and prayer, this journey would not have been possible.

# **TABLE OF CONTENTS**

THI	ESIS DECLARATION	i
ACI	KNOWLEDGEMENT	ii
TAI	BLE OF CONTENTS	iii
LIS	T OF TABLES	vi
LIS'	T OF FIGURES	viii
LIS	T OF ABBREVIATIONS	xii
LIS	T OF SYMBOLS	xiv
ABS	STRAK Jed	XV
ABS	STRACT	xvi
CHA	APTER 1 INTRODUCTION	1
1.1	Introduction	1
1.2	O Problem Statement	2
1.3	Motivation	5
1.4	Objectives	7
1.5	Scope of Research	7
1.6	Original Contribution	8
1.7	Thesis Organisation	9

CHA	CHAPTER 2 LITERATURE REVIEW 10	
2.1	Introduction	10
2.2	Frequency Bands for In-Body Wireless Biomedical Devices	11
2.3	Antenna Design for In-Body Wireless Biomedical Devices	17
2.4	Patient Safety and Exposure Standard	22
2.5	Human Body Tissue Models	26
2.6	Recent Commercial Products	31
2.7	Summary	32
	i elle	
CHA	APTER 3 METHODOLOGY	35
3.1	Design Methodology	35
3.2	Simulations setups	42
3.3	Antenna configuration	44
3.4	Measurement Setups	46
3.5	Summary	54
CHA	APTER 4 RESULTS AND DISCUSSION	55
4.1	Parametric Study	55

4.2 Resonance Characteristics 59

4.3Radiation Performance64

4.4SAR Distributions and Power Restrictions66

4.5	Communication Link Performance	74
4.6	Summary	78

<b>CHAPTER 5 CONCLUSIONS AND FUTURE WORKS</b>	79
5.1 Conclusion	79
5.2 Future Works	80
REFERENCES	82
APPENDIX – A	90
APPENDIX – B	91
APPENDIX – C	92
LIST OF PUBLICATIONS	93

# LIST OF TABLES

NO.		PAGE
2.1	The operating frequency bands for in-body wireless biomedical devices according to IEEE 802.15.6.	12
2.2	The UWB operating frequency bands for in-body wireless biomedical devices.	12
2.3	Classification of antenna research studies according to frequency bands.	15
2.4	Antenna types reported in the literature for implantable and ingestible antennas.	18
2.5	The miniaturization techniques of patch antenna design for in-body wireless biomedical devices reported in the literature.	21
2.6	ICNIRP 1998 standards.	24
2.7	IEEE C95.1-1999 standards	24
2.8	Comparisons of ICNIRP 1998 guidelines with the IEEE C95.1-2005	25
2.9	Virtual Family and Virtual Classroom human body model information.	28
2.10	Comparisons of human body tissue models used in the literature.	29
2.11	Recent commercial products regarding in-body wireless biomedical devices.	31
2.12	Comparisons of selected commercial products for ingestible wireless biomedical device in term of technical specification.	32
3.1	Basic methods and techniques used for designing in-body antenna.	37
3.2	Proposed methodology and technique.	38
3.3	Meshcells comparison.	38
3.4	Tissue dimensions and electrical properties at 2.45 GHz.	42
3.5	Detailed dimensions of proposed antenna.	46

3.6	Comparison of dielectric properties between small intestine and MSL2450.	50
3.7	Comparisons of phantom used for measurements at 2.45 GHz ISM band.	51
4.1	Summary of the optimized radiating elements dimensions.	55
4.2	Comparison of the antenna compactness based on achievable bandwidth per unit volume (by including the dielectric permittivity and the measured resonance frequency into account)	63
4.3	Simulated far-field gain achieved at 2.45 GHz ISM band.	65
4.4	Comparison of simulated far-field gain achieved at 2.45 GHz ISM band between work reported in literature and work in this thesis.	65
4.5	Maximum 1g-averaged and 10g-averaged SAR with net input power of 1 W.	66
4.6	Comparison of maximum simulated 1g-avg and 10g-avg SAR for net input power of 1W, and maximum allowable net input power inflicted by IEEE C95.1-1999 and IEEE C95.1-2005 standards at 2.45 GHz between work reported in literature and work in this thesis.	73
(1	o this item is pre	

# LIST OF FIGURES

NO		PAGE
1.1	The traditional upper and lower endoscopy procedures neglecting small intestines. Human body image is taken from ("Animated Dissection of Anatomy for Medicine (A.D.A.M),").	3
1.2	The operation of ingestible wireless biomedical device. Human body image is taken from ("Animated Dissection of Anatomy for Medicine (A.D.A.M),").	4
1.3	Ingestible wireless biomedical device layout.	5
2.1	<ul> <li>(a) The spiral patch and serpentine patch from (Soontornpipit et al., 2004),</li> <li>(b) Meandered patch from (Li-Jie et al., 2012), and</li> <li>(c) hook-shaped slot from (W. C. Liu et al., 2008).</li> </ul>	21
2.2	SAR standards by geographical regions (image from Dr Ken Joyner presentation, chairman of Regulatory Working Group, Mobile Manufacturers Forum association).	24
2.3	HUGO body model.	28
2.4	Virtual Family and Virtual Classroom models. From left to right: Duke, Ella, Billie, Thelonious, Louis, Eartha, Dizzy and Roberta.	28
2.5	<ul> <li>(a-c) The single layer canonical tissue model, multilayer canonical tissue model and anatomical tissue model from (Kiourti &amp; Nikita, 2012),</li> <li>(d) tissue simulating liquid from (Li-Jie et al., 2012) and gel mimicking tissue from (Karacolak et al., 2008).</li> </ul>	29
2.6	<ul> <li>Example of selected ingestible wireless biomedical devices available in the market:</li> <li>(a) PillCam - Given Imaging, Israel,</li> <li>(b) EndoCapsule - Olympus America, U.S,</li> <li>(c) Intellicap - Philips', Holland, and</li> <li>(d) MiroCam - IntroMedic, South Korea.</li> </ul>	33
3.1	Method 1.	35
3.2	Method 2.	36

3.3	Meshcells comparison between human body models used in simulation process using CST Microwave Studio.	39
3.4	The flowchart of the proposed design methodology for ingestible antenna proposed in the thesis.	41
3.5	Simulation setups of the proposed antenna: (a) inside 100 x 100 x 60 mm <sup>3</sup> BTSL phantom box, (b) inside 200 x 200 x120 mm <sup>3</sup> BTSL phantom box, and (c) inside 4-layer canonical tissue model.	43
3.6	The geometry of the proposed PIFA model: (a) 3D view, (b) side view, (c) ground plane, (d) lower patch, and (e) upper patch.	44
3.7	<ul><li>(a) Make a sketch on the copper tape according to the upper patch dimension.</li><li>(b) Use some of the copper tape to make the shorting-plate and cut it according the width of the lower patch. Apply both shorting-plate and upper patch to the antenna.</li></ul>	47
3.8	<ul><li>(a) Comparisons of cutting made by laser machine and Victor VR1200B.</li><li>(b) The Victor VR1200B CNC machine.</li></ul>	48
3.9	<ul><li>(a) Epoxy used in the fabrication of proposed antenna.</li><li>(b) Size comparison with United Kingdom 1p coin and the Malaysian 10 cent coin.</li></ul>	48
3.10	<ul> <li>(a) The MSL2450 body tissue simulating liquid.</li> <li>(b) Two box filled with 100x100x60 m<sup>3</sup> and 200x200x120 mm<sup>3</sup> of MSL2450 liquids, and</li> <li>(c) The fabricated antenna inside the liquid during measurement.</li> </ul>	49
3.11	The MSL2450 properties measured using Agilent FieldFox Handheld RF and Microwave Analyzer from ("Keysight Technologies,").	50
3.12	<ul><li>(a) The 'in liquid' SAR probe and probe amplifier used in the SAR measurement.</li><li>(b) The fabricated antenna during SAR measurement.</li><li>(c) SAR result showed in the CheckSAR software</li></ul>	52
3.13	Full measurement setups for: (a) S-parameter measurement and (b) SAR measurement	53

4.1	Parametric study of different width of rectangular patch $(P_w)$ .	56
4.2	The parametric study of different value of x-radius peanut-shape patch ( $R_2$ and $R_3$ ).	56
4.3	The parametric study of different value of y-radius of peanut-shape patch ( $R_1$ and $R_4$ ).	57
4.4	Simulated $ S_{11} $ of different Eccostock HiK500F dielectric constant inside a 100x100x60 mm <sup>3</sup> phantom box filled with BTSL.	58
4.5	Simulated $ S_{11} $ of antenna with shorting-pin and shorting-plate inside a 100x100x60 mm <sup>3</sup> phantom box filled with BTSL.	58
4.6	Comparison of $ S_{11} $ for simulation and measurement in 100x100x60 mm <sup>3</sup> BTSL phantom box.	59
4.7	Comparison of $ S_{11} $ for simulation and measurement in $200x200x120 \text{ mm}^3$ BTSL phantom box.	60
4.8	Comparison of $ S_{11} $ for simulation in the BTSL phantom box and 4-layer canonical model.	61
4.9	Comparison of $ S_{11} $ for different experimental setups at 2.45 GHz.	61
4.10	<ul> <li>Simulated 3-D far-field gain radiation patterns of the proposed antenna inside the:</li> <li>(a) 100x100x60 mm<sup>3</sup> BTSL phantom box,</li> <li>(b) 200x200x120 mm<sup>3</sup> BTSL phantom box,</li> <li>(c) small intestine canonical model,</li> <li>(d) small intestine + muscle canonical model,</li> <li>(e) small intestine + muscle + fat canonical model, and</li> <li>(f) small intestine + muscle + fat + skin canonical model.</li> </ul>	64
4.11	Variation in net input power for characterizing the maximum SAR (at 2.45 GHz) allowed to conform with the IEEE C95.1-1999 standard.	68
4.12	Variation in net input power for characterizing the maximum SAR (at 2.45 GHz) allowed to conform with the IEEE C95.1-2005 standard	68
4.13	Local SAR distribution at 2.45 GHz on the yz, xz and xy slices of the BTSL model (100x100x60 mm <sup>3</sup> ) and canonical model with net input power of 9.5 mW and 7.5 mW, respectively, to satisfy IEEE C95.1-1999 limitation.	69

4.14	Local SAR distribution at 2.45 GHz on the yz, xz and xy slices of the BTSL model (100x100x60 mm <sup>3</sup> ) and canonical model with net input power of 35 mW and 29 mW, respectively, to satisfy IEEE C95.1-2005 limitation.	70
4.15	The maximum SAR evaluation along the line simulation setup.	71
4.16	Maximum SAR along the line for the net input power of 1 W.	72
4.17	Maximum SAR along the line for the net input power that conforms to the IEEE C95.1-1999 and IEEE C95-2005.	
4.18	Empty space in anatomical small intestine of HUGO body model.	73
4.19	<ul> <li>(a) Simulation setups to assess the communication link performance for antenna inside BTSL and canonical models, and</li> <li>(b) circular patch antenna used as receiving antenna (Rx).</li> </ul>	75
4.20	Simulated coupling coefficient, $ S_{21} $ at 2.45 GHz for the net input power according to the IEEE C95.1-1999 and the IEEE C95.1-2005 guidelines.	76
4.21	Simulated coupling coefficient, $ S_{21} $ at different tissue layers of the canonical model with net input power that satisfy IEEE C95.1-1999 guideline.	77
4.22	Simulated coupling coefficient, $ S_{21} $ at different tissue layers of the canonical model with net input power that satisfy IEEE C95.1-2005 guideline.	77
5.1	Low power, high-speed image transmitter from (M. R. Basar et al., 2013)	81
(		

# LIST OF ABBREVIATIONS

3D	Three-Dimensional
AWGN	White Gaussian Noise
BTSL	Body Tissue Simulating Liquid
BW	Bandwidth
CST	Computer Simulation Technology
СТ	Computer Tomography
DGBE	Diethylene Glycol Butyl Ether
ETSI	European Telecommunications Standards Institute
ERM	Electromagnetic compatibility and Radio spectrum Matters
E-field	Electric Field
FCC	Federal Communication Commission
GHz	Giga Hertz
GI	Gastrointestinal Tract
H-field	Magnetic Field
ICNIRP	International Commission on Non-Ionizing Radiation Protection
IEEE	Institute of Electrical and Electronics Engineers
ISM	Industrial, Scientific and Medical
LED	Light-Emitting Diodes
MCMC	Malaysia Communications and Multimedia Commission
MHz	Mega Hertz
MICS	Medical Implant Communication System
MRI	Magnetic-Resonance Imaging
PIFA	Planar Inverted-F Antenna
RF	Radio Frequency
SAR	Specific Absorption Rate
SI	Small Intestine
SNR	Signal Noise Ratio
SRD	Short Range Devices

ULP-AMI Ultra-Low Power Active Medical Implants

ULP-AMI-P Ultra-Low Power Active Medical Implants and Peripherals

- UWB Ultra Wide-band
- Wi-Fi Wireless Fidelity
- WLAN Wireless Local Area Network

o this item is protected by original copyright

# LIST OF SYMBOLS

λ	Wavelength
С	Speed of light
dB	Decibel
ε <sub>r</sub>	Relative dielectric constant
$\mathcal{E}_{e\!f\!f}$	Effective permittivity
/ <i>E</i> /	RMS electric field
f	Frequency
g	Gram
$H_{e\!f\!f}$	Effective height
kg	Kilogram
mm	Millimetre
Ν	Noise power
σ	Electrical conductivity
ρ	Density 200
S	Mean signal
$ S_{11} $	Reflection coefficient
<i>S</i> <sub>21</sub>	Coupling strength
W	Watt
$V_d$	Volume by including dielectric permittivity and resonance frequency
<pre>/h/</pre>	
$\bigcirc$	

#### Antenna Satah Terkalih-F (ASTF) Kompak untuk Sistem Biotelemetri

#### ABSTRAK

Pendarahan dari saluran gastrousus (SG) adalah masalah perubatan umum.. SG bermula dari mulut, menuju ke esofagus, perut, usus kecil, kolon dan berakhir di rektum dan anus. Endoskopi berwayar tradisional memungkinkan ia mengdiagnos esofagus, perut, kolon, rektum dan anus, akan tetapi disebabkan limitasi fizikal, ia meninggalkan usus kecil vang sepanjang 20 kaki, tidak kira dengan menggunakan proses endoskopi dari atas atau bawah. Sebuah peranti bioperubatan tanpa wayar boleh-telan atau kapsul endoskop tanpa wayar yang dipasang dengan kamera video kecil dan cukup kecil untuk ditelan boleh memeriksa tanpa sakit bahagian-bahagian yang endoskopi berwayar tidak dapat sampai untuk memeriksa pendarahan yang tidak diketahui atau keabnormalan lain. Permintaan mencabar terhadap prestasi peranti bioperubatan tanpa wayar bolehtelan mencerminkan kesukaran dalam merekabentuk antena untuk peranti sebegitu disebabkan antena memainkan peranan penting kerana mempunyai banyak pautan komunikasi yang berkualiti dan pengecilan keseluruhan peranti, berbanding dengan komponen-komponen penting yang lain. Dalam tesis ini, satu antenna satah terkalih-F (ASTF) dicadangkan untuk diintegrasikan dengan sistem antena tablet boleh-telan untuk aplikasi biotelemetri dalam jalur industri, saintifik dan perubatan (ISP) 2.4-2.48 GHz. Dengan mengambil ciri-ciri tisu dan kerugiannya, reka bentuk antena yang dicadangkan telah dilakukan di dalam kotak dipenuhi dengan cecair simulasi tisu badan (CSTB) ( $\varepsilon_r$  = 52.7). Selain mengurangkan masa simulasi, ia juga adalah disebabkan oleh kemudahan yang praktikal untuk mengesahkan dan mengukur prestasi yang sama dalam lingkungan persekitaran yang usus kecil manusia ( $\varepsilon_r = 54.4$ ). Antena yang dicadangkan adalah padat dan disaizkan pada 859 mm<sup>3</sup> (15 mm x 12 mm x 4,7748 mm). Ia dibina menggunakan dua struktur bersusun; substrat Taconic TLY-5 ( $\varepsilon_r = 2.2$ , tan  $\delta = 0.0009$ ) dan bahan seramik Eccostock HiK500F ( $\varepsilon_r = 30$ , tan  $\delta = 0.002$ ). Ciri resonans, prestasi radiasi, pengedaran kadar penyerapan spesifik (KPS) dan pautan komunikasi antena yang dicadangkan dalam CSTB dinilai dan dibandingkan dengan prestasinya dalam empat lapisan mode tisu kanonikal (kulit, lemak, otot dan usus kecil). Yang paling penting, antena vang dicadangkan mencapai jalur lebar per unit isipadu tertinggi  $(BW/V_d)$ berbanding dengan kerja yang lain dalam literatur untuk aplikasi dalam badan.

#### Compact Ingestible Planar Inverted-F Antenna (PIFA) for Biotelemetry Systems

# ABSTRACT

Bleeding from the gastrointestinal (GI) tract is a common medical problem. The GI tract starts at the mouth, going to the oesophagus, stomach, small intestine, colon and end at the rectum and anus. The traditional wired endoscopy made it possible to diagnose the oesophagus, stomach, colon, rectum and anus, but limited by physical reasons, leaving the remaining 20 feet of the small intestines regardless using upper or lower endoscopy procedures. An ingestible wireless biomedical device or wireless capsule endoscope fitted with a mini video camera and small enough to swallow can painlessly examine the parts that wired endoscopy cannot reach for diagnosing unexplained bleeding or other abnormalities. The challenging demand of ingestible wireless biomedical device performance reflects on the difficulties of designing the antenna for those device since the antenna plays a key role for having an abundance of quality communication links and miniaturization of the whole device, compared to the other essential components. In this thesis, a compact planar inverted-F antenna (PIFA) is proposed to be integrated with an ingestible tablet antenna system for biotelemetry application in the 2.4-2.48 GHz industrial, scientific, and medical (ISM) band. By taking the tissue properties and its losses, the design of the proposed antenna was performed inside a phantom box filled with body tissue simulating liquid (BTSL) ( $\varepsilon_r = 52.7$ ). Besides reducing simulation time, this is mainly due to the practical ease to validate and measure its similar performance within the environment of a human small intestine ( $\varepsilon_r = 54.4$ ). The proposed antenna is compact and is sized at 859 mm<sup>3</sup> (15 mm x 12 mm x 4.7748 mm). It is built using twostacked structures; Taconic TLY-5 ( $\varepsilon_r = 2.2$ , tan  $\delta = 0.0009$ ) substrate and Eccostock HiK500F ceramic material ( $\varepsilon_r = 30$ , tan  $\delta = 0.002$ ). The resonance characteristic, radiation performance, specific absorption rate (SAR) distribution and communication link of the proposed antenna inside the BTSL is evaluated and compared with its performance inside a four-layer canonical tissue model (skin, fat, muscle and small intestine). Most importantly, the proposed antenna achieved the highest bandwidth per unit volume  $(\mathbf{BW}/V_d)$  compared to other work in literature for in-body applications.

#### **CHAPTER 1**

#### **INTRODUCTION**

# 1.1 Introduction

For several decades, electromagnetism has been popular and continuously used in medical application such as microwave imaging, breast tumour detection, diagnosis, cancer treatment and many more (Rosen, Stuchty, & Vander Vorst, 2002). Nowadays, in the modern medical application, the wireless capabilities in electromagnetism world are extremely useful especially in biological telemetry (biotelemetry) application for diagnostic purposes. The biotelemetry is defined as transmitting biological or physiological information from inaccessible location to a remote monitoring site that has capability to interpret the data and affect decision making (Güler & Übeyli, 2002). The wireless biomedical devices for such biotelemetry system that can be used deeper inside the human body and transmit information to a receiver outside the body is no longer be the stuff of science fiction. A recent in-body wireless biomedical device that is gaining a lot of attention due to the capabilities of enabling the monitoring within the human body is the ingestible wireless biomedical device for endoscopy or sometimes called wireless capsule endoscopy.

## **1.2 Problem Statement**

Most diseases such as ulcer, tumour or tissue bleeding will degenerate into cancer or some other critical diseases if not cured or controlled in their early stages, but it is not that easy to diagnosing all these diseases due to lack of specific equipment or technologies. The angiography, ultrasonography, X-radiography or other current technologies used to detect such diseases in the gastrointestinal (GI) tract were reported to give low diagnostic outputs for bleeding detection (Lewis, 2000; Zuckerman, Prakash, Askin, & Lewis, 2000), unless the bleeding become severely active (Howarth, Tang, & Lees, 2002). Bleeding from the GI tract is a common medical problem and the tract is a long, hollow, muscular passage where food and nutrients passes and absorbed. It starts at the mouth, going to the oesophagus, stomach, small intestine, colon and end at the rectum and anus. The traditional wired endoscopy made it possible to diagnose the oesophagus, stomach, colon, rectum and anus, but limited by physical reasons, leaving the remaining 20 feet of the small intestines regardless upper or lower endoscopy procedures as shown in Figure 1.1. Additionally, the use of wired endoscopy is usually very inconvenient for the patients, cause an intense pain and can increase the risk of having cross-contamination.



Figure 1.1: The traditional upper and lower endoscopy procedures neglecting small intestines. Human body image is taken from ("Animated Dissection of Anatomy for Medicine (A.D.A.M),").

An ingestible wireless biomedical device or wireless capsule endoscope fitted with a mini video camera and small enough to swallow can painlessly examine the parts that wired endoscopy cannot reach for diagnosing unexplained bleeding or other abnormalities (Mylonaki, Fritscher-Ravens, & Swain, 2003). The video data is transmitted wirelessly (as shown in Figure 1.2) and directly to a receiver or to a recorder attached to the patient's abdomen and later downloaded onto a computer for analysis.



Figure 1.2: The operation of ingestible wireless biomedical device. Human body image is taken from ("Animated Dissection of Anatomy for Medicine (A.D.A.M),").

From the analysis, doctors or physicians able to make early, accurate diagnosis problems and make appropriate treatment. The patient also can relax in comfort without a hospital stay. There is no sedation involved during the procedure and additional investigations can often be avoided. Typical ingestible wireless biomedical device system contains many components as shown in Figure 1.3 including antenna, transmitter, batteries, camera, short focal length lens, light-emitting diodes (LED), lens holder and optical dome.



Figure 1.3: Ingestible wireless biomedical device layout.

by original

#### 1.3 Motivation

The challenging demand of in-body wireless biomedical device performance reflects on the difficulties of designing the antenna for those devices since the antenna plays a key role for having an abundance of quality communication links and miniaturization of the whole device, compared to the other essential components. In many ways, the design of antennas for the ingestible wireless biomedical device is similar to the design of antennas for implantable biotelemetry application in general, and there are some several requirements and challenging issues in designing these types of antenna:

- a) Size constraints: The size of the antenna has to be very small and minimized as the antenna supposed to fit in dense packaging that also includes other essential components as the whole device is intended to operate in the human body.
- b) Wide bandwidth: The antenna has to radiate into a complex lossy environment (human body) rather than into free space, thus antenna performance becomes

dependent on the surrounding tissue type with different layers and dielectric properties. Therefore, the antenna need to have a wide bandwidth to withstand the frequency shifting caused by those environments.

- c) Radiation and coupling performance: The radiation characteristic of an antenna may have standard definitions (Balanis, 2012). However, the gain of the antenna for this type of application usually low due to the losses in the tissue and it is very difficult to get the radiation performance near to the ideal lossless antenna. Therefore, the communication link in terms of coupling between antenna inside the body and external receiving unit need to be evaluated to ensure the communication robustness.
- d) Patient safety: Due to the fact that the radiation and propagation of the antenna from inside to the outside of the human body will cause the rise of temperature in the body tissues, the antenna has to comply with the maximum specific absorption rate (SAR) set by certain regulators and standards.

Motivated in part by the need of new antenna for ingestible wireless biomedical device that have a wide bandwidth, compact and at the same time can deal with patient safety, this thesis aims to design an ingestible antenna at 2.4 GHz - 2.48 GHz ISM band, since this band have the most potential to become promising solutions to be used for the in-body wireless biomedical devices inside the human body as the frequency band being well-developed in terms of technology (i.e: Wi-Fi) and favourable for high data rate applications such as real-time video transmission. Recent commercial products operate at 433 MHz and such lower frequency may give an advantage on propagation to an outside body, but not able to support high data rate communication and high quality real-time continuous image transmission.