HUMAN BODY'S CHANNEL MODELING AND LOW POWER, HIGH DATA RATE TRANSCEIVER DESIGN FOR WIRELESS CAPSULE ENDOSCOPY

MD. RUBEL BASAR CONVIENT
MD DIDEL DASAD
WID. KUDEL BASAK
Or Poi
9.07
xecte
e e e e e e e e e e e e e e e e e e e
ents
hisite

UNIVERSITI MALAYSIA PERLIS

2013



HUMAN BODY'S CHANNEL MODELING AND LOW POWER, HIGH DATA **RATE TRANSCEIVER DESIGN FOR WIRELESS CAPSULE ENDOSCOPY** by rightal copyright by rightal copyright

MD. RUBEL BASAR

(1130810707)

This item is protect A thesis submitted in fulfilment of the requirement for the degree of Master of Science (Communication Engineering)

SCHOOL OF COMPUTER AND COMMUNICATION ENGINEERING **UNIVERSITI MALAYSIA PERLIS**

2013

UNIVERSITI MALAYSIA PERLIS

	DEC	CLARATIO	N OF THESIS			
Author's full name	Author's full name : Md. Rubel Basar					
Date of birth	: 26 th June, 19	986				
Title		•	Modelling and Low Power, High Data for Wireless Capsule Endoscopy			
Academic session	: 2012-2013					
-			he property of Universiti Malaysia Perlis UniMAP. This thesis is classified as:			
		ontains con cret Act 1972	fidential information under the Official 2)			
	,	(ricted information as specified by the here research was done)			
$\bigvee \text{OPEN ACC}$	L L		thesis is to be made immediately available online open access (full text)			
I, the author give permission to the UniMAP to produce this thesis in whole or in part for the purpose of research or academic exchange only (except during the period of years, if so requested above). Certified by:						
SIG	SNATURE		SIGNATURE OF SUPERVISOR			
Md.Rubel I	Basar (E024492	29)	Dr. Mohd Fareq Bin Abd Malek			
(NEW IC I	NO. / PASSPO	ORT NO.)	NAME OF SUPERVISOR			
Date:			Date:			

ACKNOWLEDGEMENT

My deepest thanks to the Almighty Allah S.W.T. (Alhamdulillah), the Omnipotent, the Merciful and the Compassionate, for giving me the strength, patience and determination in compiling this research. Then, I would like to express my gratefulness to my supervisor, Dr. Mohd Fareq bin Abd Malek for his valuable and constructive suggestions thought this thesis that enabled it to run smoothly. Prof. Dr. R. Badlishah Ahmad provided excellent research facilities under the school of computer and communication engineering. I also deeply grateful to the Ministry of Higher Education, Malaysia, for providing financial support for this thesis work under the grant FRGS/FASA/TAHUN/SKK/JPP/03/6 via Politeknik Tuanku Syed Sirajuddin and Khairudi Mohd Juni for managing this grand. I would like to share this moment of contentment and express the appreciations to my parents who were encouraged at every step in my life. I am very much indebted to my cousin Md. Azabul Haque, for his guidance and great source of motivation in my higher study. I owe a special gratitude to the Bangladesh community in Perlis specially to Dr. Fazlul Bari and Md. Mohiuddin for their mental support. Finally, I thank everyone else who has facilitated the making of this thesis, including other colleagues.

MD. RUBEL BASAR

UNIVERSITI MALAYSIA PERLIS (UniMAP) rubel24434@gmail.com

TABLE OF CONTENT

DECLARATION OF THESIS	i
ACKNOWLEDGEMENT	ii
TABLE OF CONTENT	iii
LIST OF TABLE	vii
LIST OF FIGURE	viii
LIST OF ABBREVIATION	xi
LIST OF SYMBOLS ABD VARIABLS	xiii
ABSTRAK (MALAY)	xv
LIST OF TABLE LIST OF FIGURE LIST OF ABBREVIATION LIST OF SYMBOLS ABD VARIABLS ABSTRAK (MALAY) ABSTRACT (ENGLISH)	xvi
CHAPTER 1: INTRODUCTION	
1.1 Background	1
1.2 Motivation for This Research	3
1.3 Thesis Objectives	4
1.4 Methodology	5
1.5 Organization of This Thesis	6

2.1	Overview of GI Endoscopy	8
2.2	Human GI Track Anatomy	9
2.3	Wireless Capsule Endoscopy	11
	2.3.1 Wireless Capsule Endoscopy System	11

	2.3.2	Pre-preparation of Wireless Capsule Endoscopy	13
	2.3.3	Present Clinical Product of Wireless Capsule	14
2.4	Batter	ry-less Capsule	19
2.5	Progre	ess Tendency of Current Wireless Capsule Endoscopy	19
	2.5.1	ASIC Design	21
	2.5.2	Capsule Actuation System	23
	2.5.3	Miniaturized Power Source	26
	2.5.4	Comments on Different Progress Tendency	28
2.6	Huma	n Body's Channel Analysis	30
2.7	Transo	Miniaturized Power Source Comments on Different Progress Tendency In Body's Channel Analysis ceiver Architecture Transmitter Topology	31
	2.7.1	Transmitter Topology	32
		2.7.1.1 Direct Conversion Transmitter	32
		2.7.1.2 Direct Modulation Transmitter	33
		2.7.1.3 Impulse Radio Transmitter	33
	2.7.2	ReceiverTopology	34
		2.7.2.1 Super-heterodyne Receiver	34
		2.7.2.2 Low-IF Receiver	35
	$\mathbf{\mathbf{\mathbf{\mathbf{\mathbf{\mathbf{\mathbf{\mathbf{\mathbf{\mathbf{\mathbf{\mathbf{\mathbf{\mathbf{\mathbf{\mathbf{\mathbf{\mathbf{$	2.7.2.3 Direct Conversion Receiver	35
		2.7.2.4 RF Analog to Digital Conversion Receiver	36
		2.7.2.5 Impulse Radio Receiver	37

CHAPTER 3: METHODOLOGY

3.1	Introduction	38
3.2	Methods of Path Loss Analysis	39
	3.2.1 Human Body Model	40

	3.2.2	Simulation Setup	43
3.3	Telem	etry System	46
3.4	Transı	nitter Design	47
	3.4.1	Transmitter Architecture	47
	3.4.2	Oscillator Design	49
	3.4.3	Operation of Current Reuse Oscillator	52
	3.4.4	Oscillator's Start-up Time Optimization	53
	3.4.5	Envelope Filter Design	54
	3.4.6	Matching Network Design	55
3.5	Receiv	ver Design	56
	3.5.1	Oscillator's Start-up Time Optimization Envelope Filter Design Matching Network Design ver Design Receiver Architecture	56
	3.5.2	Link Budget Calculation	57
	3.5.3	LNA Design	58
	3.5.4	Logarithmic Amplifier, Rectifier and Comparator Circuit Design	62

CHAPTER 4: RESULT AND DISCUSSION

4.1	Introd	uction	65
4.2 (Huma	n Body's Channel Modelling	66
	4.2.1	Path-loss In Human Body's Channel	66
	4.2.2	Optimum Frequency for Wireless Capsule Endoscopy	71
4.3	Simul	ated Results of Direct Modulation Transmitter	74
	4.3.1	Oscillator's Characteristics	74
	4.3.2	Start-up Time Optimization	77
	4.3.3	Envelope Filter	79
4.4	Simul	ated Results of Receiver	83

	4.4.1	LNA Simulation Results	83
	4.4.2	Limiting Amplifier Simulation Result	86
	4.4.3	Detector and Comparator	87
4.5	Summ	nary	89

CHAPTER 5: CONCLUSION AND FUTURE WORKS

5.1	Conclusion and Research Findings	91
5.2	Suggestions for Future Works	93
	Conclusion and Research Findings Suggestions for Future Works ERENCES ENDICES Appendix A: TSMC 0.18 un CMOS Process Parameter	94
APP	ENDICES	
	Appendix A: TSMC 0.18 µm CMOS Process Parameter	106
	Appendix B: Publications	111
	Appendix B: Publications	
(OTHISIL	

LIST OF TABLES

NO.	CAPTION	PAGE
Table 2.1	Specification of current wireless endoscopic capsules.	18
Table 2.2	Development of miniaturization technology.	29
Table 3.1	Electrical properties of used heterogeneous human body model.	41
Table 3.2	Description of the capsule locations used in the investigation of path loss.	44
Table 3.3	Low-power techniques used in the architecture of the proposed transmitter.	48
Table 3.4	Value of circuit elements used in transmitter system.	56
Table 3.5	The Link budget of the proposed OOK system for wireless capsule endoscopy.	58
Table 3.6	Optimum component size (Parameter value) of LNA.	61
Table 3.7	The component's size of the above circuit diagram.	64
Table 4.1	The frequency range that was considered in the simulation of the properties of specific tissue.	66
Table 4.2	Minimum and maximum path loss throughout the capsule's path.	72
Table 4.3	Minimum and maximum path loss at frequencies of 450 MHz and 900 MHz.	73
Table 4.4	Performance shifting of transmitter with different V-high values.	82
Table 4.5	Performance comparison of proposed telemetry system	90

LIST OF FIGURES

NO.	CAPTION	PAGE
Figure 2.1	Architecture of human GI tract with wireless capsule.	10
Figure 2.2	(a) Internal architecture of endoscopic capsule 1. Optical dome; 2. Lens holder; 3. Lens 4. LEDs; 5. COMS imager 6. Battery; 7. ASIC transceiver; 8. Antenna, (b) Image receiving antenna leads with the image storage device, (c) Image analyzing workstation.	12
Figure 2.3	Common set up of antenna leads on the patient's body.	13
Figure 2.4	Present clinical capsules: (a) PillCam SB; (b) PillCam Eso; (c) PillCam Colon; (d) OMOM; (e) Olympus; (f) MiroCam.	14
Figure 2.5	The difference between PillCam SB and SB2 (view angle and covered area).	16
Figure 2.6	Real time display with data recorder.	16
Figure 2.7	Architecture of the battery-less capsules (a) Norika and (b) Sayaka capsule.	20
Figure 2.8:	Prototype of an FPGA-based, miniaturized capsule.	22
Figure 2.9	Capsule actuation mechanisms (a) Leg based (b) Magnetic theory based (c) Electrical stimulation based.	24
Figure 2.10	(a) Wireless power transmission system; (b) 3D power receiving coil with rectifier circuit.	26
Figure 2.11	Typical direct conversion transmitter architecture.	32
Figure 2.12	Simplified direct modulation transmitter architecture.	34
Figure 2.13	Schematics of impulse radio transmitter.	34
Figure 2.14	Single down conversion super-heterodyne receiver architecture.	35
Figure 2.15	Simplified Direct conversion architecture.	36
Figure 2.16	Digitalized with RF analog to digital conversion receiver.	36
Figure 2.17	Impulse radio receiver.	37
Figure 3.1	Heterogeneous model of the human body.	43
Figure 3.2	Human anatomy used in the body model showing the capsule	44

locations that were considered in investigating the path loss.

Figure 3.3	(a) Simulation setup for investigating the path loss in the body channel; (b) boundary condition.	45
Figure 3.4	Variation of accuracy with the resolution of body model in simulation.	46
Figure 3.5	Analogy of on off-keying telemetry system.	47
Figure 3.6	Architecture of proposed, low power, high speed transmitter.	48
Figure 3.7	Proposed transmitter circuit.	50
Figure 3.8	Operation of VCO during (a) positive half, and (b) negative half cycle of output.	52
Figure 3.9	Response of the oscillator to a pulse input.	54
Figure 3.10	Block diagram of proposed receiver system.	56
Figure 3.11	Circuit diagram of LNA.	59
Figure 3.12	(a) The smith chart of input matching, (b) The smith chart of output matching.	61
Figure 3.13	Logarithmic amplifier, power detector and comparator.	63
Figure 4.1	Path loss for the capsule position at A (upper esophagus).	67
Figure 4.2	Path loss for the source position at B (lower esophagus).	68
Figure 4.3	Path loss for the source position at C (stomach).	68
Figure 4.4	Path loss for the source position at D (upper intestine).	70
Figure 4.5	Path loss for the source position at E (upper abdominal region).	70
Figure 4.6	Path loss for the source position at F (abdominal region).	71
Figure 4.7	Variation of path loss in the human body's channel.	73
Figure 4.8	(a) Oscillator phase noise; (b) Carrier spectrum (at a frequency of 450 MHz).	75
Figure 4.9	OOK-modulated signal at three data transmission rates: (a) 20 Mb/s, (b) 40 Mb/s, (c) 100 Mb/s.	76
Figure 4.10	Optimized start-up time for the oscillator: (a) Performance before capacitance matching (solid curve) and after capacitance matching (dashed curve); (b) Performance before tank circuit optimization (solid curve) and after tank circuit optimization (dashed curve).	78

Figure 4.11	OOK-modulated signal after optimizing start-up time at (a) 20 Mb/s, (b) 40 Mb/s, (c) 50 Mp/s, and (d) 100 Mb/s.	79
Figure 4.12	OOK-modulated signal after the envelop filter at (a) 20 Mb/s, (b) 40 Mb/s, (c) 50 Mp/s, and (d) 100 Mb/s.	80
Figure 4.13	Signal spectra of envelope filtered signal at (a) 20 Mb/s, (b) 40Mb/s, (c) 50 Mp/s, and (d) 100 Mb/s.	81
Figure 4.14	Reflection coefficient of matching network.	82
Figure 4.15	Simulated reflection loss of input matching (S11) and output matching (S22) of LNA.	83
Figure 4.16	Simulated forward gain of the LNA.	84
Figure 4.17	Input output isolation of LNA, in terms of forward gain and backward gain.	85
Figure 4.18	Noise figure of LNA.	85
Figure 4.19	The 1 dB compression point (IP1) of LNA.	86
Figure 4.20	Gain characteristics of logarithmic amplifier (LA) at the output of different stage.	87
Figure 4.21	The DC voltage level of the rectified signal from LA3 corresponding the input signal from -100 dBm to 0 dBm.	88
Figure 4.22	Comparator output over the dynamic range of input signal.	88
Figure 4.23	Received input power vs receiver's output voltage.	89
©		

LIST OF ABBREVIATIONS

ADS	Advanced design system
AGC	Automatic gain control
ASIC	Application specific integrated circuit
ASK	Amplitude shift keying
BER	Bit error rate
CCD	Bit error rate Charge-coupled device Complementary metal oxide semiconductor Computer simulation technology
CMOS	Complementary metal oxide semiconductor
CST	Computer simulation technology
СТ	Computer tomography
DOF	Degree of freedom
EM	Electromagnetic
FCC	Federal communication commission
FDA	Food and drug administration
FDTD	Finite difference time domain
FIT	Finite integration technique
FSK	Frequency Shift Keying
GI	Gastrointestinal
IF	Intermediate frequency
IR-UWB	Impulse radio ultra wide band
LA	Logarithmic amplifier
MRI	Magnetic resonance imaging
NF	Noise figure
OGIB	Obscure gastrointestinal bleeding
OOK	On off keying

- Phase locked loop PLL
- Radio frequency RF
- SNR Signal to noise ratio
- TSMC Taiwan semiconductor manufacturing company
- VCO Voltage control oscillator
- WBAN Wireless body area network
- WCE
- WPT

o This item is protected by original copyright

LIST OF SYMBOLS AND VARIABLES

P_t	Transmitted power
P_r	Received power
d	Distance between the transmitting point and the receiving point
f	Frequency
С	Speed of light
$\overline{\mathcal{E}}_r$	Relative permittivity
$\overline{\sigma}$	Speed of light Relative permittivity Conductivity Attenuation constant of body tissue
$lpha_{\scriptscriptstyle body}$	Attenuation constant of body tissue
L_{body}	Path loss by the body tissue
d_{body}	Distance between the source and the receiving antenna in WCE
μ	Permeability NMOS
MN	NMOS
MP	PMOS.
L	Inductance
C	Capacitance
K	Boltzmann's constant,
T	Absolute temperature,
A	Start-up safety factor
\mathcal{O}_{o}	Frequency of oscillation
$\Delta \omega$	Offset frequency
V	Peak output amplitude
Q	Quality factor
W_M	Width of active device
L_M	Length of active devices

- Carrier's mobility of P-type/N-type material $\mu_{p/n}$
- C_{ox} Gate capacitance per unit area
- Start-up period of oscillator t_{s-u}
- Steady-state period of oscillator t_{s-s}
- Decay period of oscillator t_d
- Transconductance of MOS transistor g_m

o This item is protected by original copyright

Permodelan Saluran Tubuh Manusia dan Rekabentuk Penghantarterima Kuasa Rendah Data Berkadar Tinggi untuk Endoskop Kapsul Wayarles

ABSTRAK

Endoskop Kapsul Wayarles (EKW) boleh hadam adalah satu-satunya teknologi diagnostik baru yang tidak menyakitkan dan efektif untuk memeriksa keseluruhan laluan penyakit gastrousus (GU). Tetapi beberapa batasan utama, resolusi imej yang teruk, masa penggunaan yang terhad dan tidak mampu untuk melihat kawasan kritikal secara berulang menghadkan penggunaan teknologi ini secara meluas. Untuk pembangunan EKW yang seterusnya, tumpuan utama ialah membangunkan sistem berkuasa rendah dan kelajuan tinggi yang mampu menghantar imej telemetri beresolusi tinggi pada kadar bingkai yang lebih tinggi. Oleh itu, tesis ini melaporkan penyiasatan kehilangan laluan dan perubahannya dalam saluran badan manusia melaluai rekabentuk penghantarterima (penghantar dan penerima) berprestasi tinggi. Untuk menyiasat kehilangan laluan dalam saluran badan, model tubuh manusia yang berbezabeza telah digunakan, yang mana lebih setanding dengan badan manusia daripada model seragam. Teknik integrasi terhingga (TIT) dalam perisian Computer Simulation Technology (CST) Microwave Studio telah digunakan dalam simulasi. Kehilangan laluan dianalisa dalam julat frekuensi 100 MHz hingga 2450 MHz. Kehilangan laluan didapati paling nyata lebih rendah pada frekuensi bawah 900 MHz. Kehilangan terkecil di sekitar frekuensi 450 MHz, di mana perubahan kehilangan didapati laluan sepanjang saluran GI adalah 29 dB, dengan minimum -9 dB dan maksimum -38 dB. Walau bagaimanapun, pada 900 MHz, perubahan ini telah diperhatikan menjadi 38 dB, dengan minimum 40 dB dan maksimum 48 dB. Kehilangan laluan menjadi agak tinggi semasa pemeriksaan di bahagian anatomi-kompleks, seperti di usus atas dan esofagus bawah berbanding dengan perut kurang kompleks dan bahagian esofagus atas. Oleh itu, adalah disyorkan bahawa spektrum yang dipusatkan pada 450 MHz menjadi pilihan yang optima bagi memihak kepada kehilangan laluan kecil. Akhirnya, sebuah pemancar modulasi langsung yang sangat cekap dan analog RF berdigital kepada penerima penukaran digital yang kedua-duaanya menyokong kadar data sehingga 100 Mbps, telah direka dalam perisian Advanced Design System (ADS) pada 450 MHz. Laluan penghantaran hanya terdiri daripada pengayun kuasa rendah, penapis terkandung dan sebuah rangkaian sepadan. Keseluruhan litar pemancar secara purata menggunakan 2 mA dari bekalan 1.5 V DC. Permulaan tempoh fasa pengayun telah dioptimumkan kepada kurang daripada 6 ns untuk menyokong penghantaran data digital pada kadar 100 Mbps. Disamping itu, penerima telah dilaksana dengan menggunakan penguat hingar rendah (PHR), penguat logaritma (PL), pengesan kuasa dan pembanding. PHR tersebut dan tiga peringkat PL memberikan gandaan sebanyak 80 dB yang menjadikan penerima dapat mengesan input isyarat yang lemah sehingga dari peringkat -80 dBm.

Human Body's Channel Modeling and Low Power, High Data Rate Transceiver Design for Wireless Capsule Endoscopy

ABSTRACT

Ingestible wireless capsule endoscopy (WCE) is one and only the painless effective novel diagnostic technology for inspecting entire gastrointestinal (GI) track diseases. But some major limitations, poor image resolution, limited working time and unable to repeated view of critical area confine the wider application of this technology. For the further development of WCE, the main concern is the development of a low power and high-speed telemetry system that is capable of transmitting high-resolution images at a higher frame rate. In this regard, this thesis report on investigation of path loss and its variation in human body channel with high performance transceiver (transmitter and receiver) design. To investigate the path loss in the body channel, a heterogeneous human body model was used, which is more comparable to the human body than a homogenous model. The finite integration technique (FIT) in Computer Simulation Technology's (CST's) Microwave Studio was used in the simulation. The path loss was analyzed in the frequency range of 100 MHz to 2450 MHz. The path loss was found to be saliently lower at frequencies below 900 MHz. The smallest loss was found around the frequency of 450 MHz, where the variation of path loss throughout the GI tract was 29 dB, with a minimum of -9 dB and a maximum of -38 dB. However, at 900 MHz, this variation was observed to be 38 dB, with a minimum of -10 dB and a maximum of -48 dB. The path loss was comparatively higher during examination of anatomically-complex regions, such as the upper intestine and the lower esophagus as compared to the less complex stomach and upper esophagus areas. Therefore, it is recommended that the spectrum centralized at 450 MHz should be the optimum selection in favour of smallest path loss. Finally, a highly efficient direct modulation transmitter and a digitalized RF analog to digital conversion receiver, both of supporting the data rate up to 100 Mbps, have been designed in Advanced Design System (ADS) at 450 MHz. The transmitting path consists only a low power oscillator, an envelope filter and a matching network. The entire transmitter circuit draws average 2 mA current from a 1.5 V DC supply. The start-up transient period of oscillator is optimized to less than 6 ns to support digital data transmission at the rate of 100 Mbps. On the other hand, the receiver is implemented using a low noise amplifier (LNA), logarithmic amplifier (LA), power detector and comparator. The LNA and the three stages LA provide the gain 80 dB which makes able the receiver sense the input weak signal up to the level -80 dBm.

CHAPTER 1

INTRODUCTION

1.1 Background

Endoscopy is a system that makes it possible to conduct visual examinations inside the body for medical reasons. Most of the lethal diseases in the gastrointestinal (GI) track such as cancer, tumors, obscure gastrointestinal bleeding (OGIB), crohn's disease, and celiac disease can be controlled and cured if it is possible to detect in their earlier stages (Pan et al., 2012). Angiography, Ultrasonography, X-radiography, computer tomography (CT), and magnetic resonance imaging (MRI) are conventional, indirect technologies for examining GI tract diseases. Regrettably, these technologies have low diagnostic yields because their inability to show the wall of the GI tract. Another typical technology, probe/wired endoscopy, is used for diagnosing diseases of the GI tract, but, in addition to being painful and creating discomfort, it is incapable of reaching some critical locations in the GI tract.

The development of ingestible wireless capsule endoscopy (WCE) is viewed as a revolutionary advancement in GI tract endoscopy. This emerging technique overcame the previous complexities associated with inspecting the entire small intestine, which is the most complex part of the GI tract and is unreachable by conventional probe endoscopy. In 2000, Iddan et. al., (2000) first developed a wireless video capsule endoscopy system that patients could swallow, but its development has been started since long ago. The concept of the swallowable wireless capsule realized with the development of parametric capsule for measuring physiological parameter of GI track such as pressure, temperature and pH. The invention of parameter capsule was possible, due to the development of the transistor that allowed to design small size radio-telemetry for capsule. However, this capsule was unable to see the GI track wall. In 1981, Iddan first developed the concept of wireless video capsule endoscopy to see the wall of the GI tract painlessly, but the state of the development of the required technology deterred the realization of this concept. Fourteen years later, Swain et. al., (1997) developed several prototypes of a capsule endoscopy system and successfully conducted a vast number of experiments on post-mortem and live pigs. In those prototypes, they used a miniature charge-coupled device (CCD) camera, a video processor, a 10-mW microwave transmitter with a 1.5-cm dipole antenna, a light source, and a battery. In 2000, the introduction of the low-power, complementary metal oxide semiconductor-based (CMOS-based) image sensor and application specific integrated circuit (ASIC) made the video capsule possible (Iddan et.al., 2000).

Since the development of this technology, several companies have made remarkable improvements in their clinical products, but there are still some limitations that relate to the use of conventional, wired endoscopy. Some of the major limitations that currently impede its wider application include its working time constraints, poor image quality and inability to repeat the view of critical areas. Many research groups currently are working on ways to solve these limitations. Developing the low power high data rate telemetry system is the most promising area of improving capsule's performance, because it can allow high speed transmission of high quality image, consuming low power which can increase also capsule's working time.

1.2 Motivation for This Research

The GI track disorder is a very common problem of human being. Due to the severe pain and discomfort in typical probe endoscopy (cannulae with embedded light source and image sensor that are inserted through the mouth, anus or nose), patients are quite sick to go through the endoscope. Along with this, the limited level of insertion of endoscopic probe makes this technology unable to view inside the small bowel (Loeve et al., 2010). In the recent past, the development of technology for low power CMOS image sensor, ASIC and miniaturized LEDs enable the realization of WCE that overcomes the downsides of conventional endoscopy (Cruti et al., 2011). However, the limited working time, lower frame rate and low image regulation deter the wider application of WCE and made still existing of probe endoscopy in the clinic. This leads to remarkable ongoing research on the further development of WCE.

The path loss by the wireless body channel, between in body capsule and on body receiving antenna, can't be readily calculated due to the complex multilayer structure of human body and the frequency dependent properties of its different tissues. Few researches have been conducted on the investigation of radiation characteristics (Alomainy et al., 2006; Alomainy et al., 2009; Chirwa et al., 2003; Takizawa et al., 2011) where the path loss and the variation of path loss with the possible capsule locations are not reported properly. Some of these researches are using a homogeneous body model which is less comparable to the actual human body than the heterogeneous body model (Ji-Hyun Jung et la., 2010; Theilmann et al., 2012). Therefore, the path loss analysis in the human body channel using a heterogeneous body model is an essential task to develop an efficient telemetry system for high quality image transmission.

After the body channel analysis, high speed radio frequency (RF) transceiver system will need to be designed which is not straightforward. In the RF system design the bandwidth of system is a vital issue as in the digital system data rate is strongly related to the system bandwidth (Lee et al., 2011). So, the bandwidth should be wider enough to support the transmission of high resolution image data. The present capsule system has the data rate around 2 Mbps (Chi et al., 2007; Itoh et al., 2006), that is able to transmit the image with the resolution of 256x256 pixel at the rate of 2 frames per second. Recently, many RF telemetry systems have been developed (Gao et al., 2011; Kim et al., 2012; Thone et al., 2009) and the maximum data rate have been achieved 20 Mbps that also not sufficient for transmitting 640x640 pixel image at the rate of 30 frames per second. Hence, a potential research is required to develop highly efficient Thesis Objectives and high data rate telemetry system.

1.3

The main purpose of this thesis is addressing the solution of the major limitations of the present WCE system those deter the wider application of WCE in clinic. Considering the practicality, to accomplish the goal, this research work opted into the following objectives:

- 1. To investigate the human body's channel condition through path loss analysis and to determine the optimum frequency spectrum for the efficient telemetry system of WCE.
- 2. To design high speed RF transmitter at the optimum frequency to support high quality image transmission at higher number of frames per second with lowest power consumption.

3. To design high speed, simplified RF receiver at the optimum frequency with sufficient bandwidth to support high speed data reception while keeping the optimum power consumption and the sufficient receiver's sensitivity.

1.4 Methodology

In order to investigate the human body's channel condition and optimum system frequency for WCE, path loss and its variation has been analyzed in heterogeneous digital body model using Computer Simulation Technology's (CST's) Microwave Studio, which based on the finite integration technique (FIT). The simulation environment is created by cutting the digital body model in a brick shape (10cm x 10cm x Dcm). Where, D is the depth of the brick and the value of D vary in the simulation from 4cm to 17cm according to the consideration of the actual depth of the capsule. Setting the boundary condition, the brick is considered virtual waveguide. Two waveguide ports were used at the opposite end of the virtual waveguide to evaluate the microwave transmission coefficient S_{21} .

Taiwan Semiconductor Manufacturing Company's RF CMOS 0.18 μ m process (version 3.0) is used in Advanced Design System (ADS) for simulating both of transmitter and receiver circuit symmetry. To ensure the low power design, the on-off keying (OOK) modulation scheme is adopted in direct modulation transmitter architecture. The current reuse oscillator is turned on and off by the transmitting bits that consequences the OOK signal. Furthermore, an envelope filter and matching network are used to filter the OOK signal and to match antenna input impedance 50 Ω . The direct RF analog to digital conversion architecture is used at the receiving end. In the receiver subsequent block, the common source cascade low noise amplifier (LNA) is designed to have a high LNA gain, reverse isolation and low noise figure (NF) and wider bandwidth. Finally, to extract the transmitted data bit, logarithmic amplifier (LA), the rectifier and the DC level comparator are added sequentially to the receiver section.

1.5 Organization of the Thesis

This thesis is organized with five distinct chapters and the contains of each chapter is as described below:

Chapter 1 demonstrates brief background of the tropic, motivation for this research, objectives and used methodology alongside this chapter cover the organization of this thesis.

Chapter 2 illustrates the present wireless endoscopic capsules those are currently using in clinic, detailed literature review of current research on the betterment of present capsule, achievement and technical challenges, and the overall discussion with the promising side of capsule to develop.

Chapter 3 describes the methods of path loss analysis in the human body's channel using digital body phantom, simulation setup to determine the path loss in terms of different frequency and location of the capsule in GI path, architectures of proposed RF transmitter and receiver, low power circuit design approach, and the design of low power high data transmitter and receiver with the optimization to enhance the data rate and to reduce the power consumption.

Chapter 4 explains the channel characteristics of human body for electromagnetic (EM) signal propagation to figure out the optimum frequency for WCE, the performance of the proposed RF transmitter and receiver in the most favorable