

PAPER • OPEN ACCESS

Image Enhancement Using Modified Partial Contrast Technique in Ziehl-Neelsen Sputum Slide Images

To cite this article: R. A. A. Raof *et al* 2019 *J. Phys.: Conf. Ser.* **1372** 012080

View the [article online](#) for updates and enhancements.



IOP | ebooks™

Bringing together innovative digital publishing with leading authors from the global scientific community.

Start exploring the collection—download the first chapter of every title for free.

Image Enhancement Using Modified Partial Contrast Technique in Ziehl-Neelsen Sputum Slide Images

R. A. A. Raof¹, M. Y. Mashor¹, S. S. M. Noor²

¹Universiti Malaysia Perlis, Pauh Putra, Perlis, Malaysia

²Universiti Sains Malaysia, Kubang Kerian, Kelantan, Malaysia

Corresponding Author E-mail: rafikha@unimap.edu.my

Abstract. Image contrast and brightness for sputum slide images are among important factors that can affect the accuracy of image analysis process. Microscopic images usually have the problem of low contrast and blurry, which are caused by a couple of factors such as uneven thickness of the slides and manual preparation of the slide in the first place. In this research, image enhancement procedure has been considered for either increasing the image quality, increasing the visibility of tubercle bacilli or to ease the segmentation process. Partial contrast technique is considered for the contrast enhancement method. The results show that the modified technique helps to improve tubercle bacilli visibility. Hence the resulted images would become useful for the microbiologists and technologists for further analysis of Ziehl-Neelsen (ZN) sputum slide.

1. Introduction

Several computer-aided image diagnosis methods for tuberculosis (TB) detection have been described in the literature [1 – 5]. These methods can be divided into two approaches: using fluorescence and light microscope. Early works focused on using the fluorescence microscope [1 - 3]. Images viewed using a fluorescence microscope is more sensitive to TB bacilli and the screening process can be conducted quickly under lower magnification, compared to the light microscope [4]. However, it is expensive and difficult to maintain, thus limiting the use of fluorescence microscope in low and medium income countries. Therefore, recent works in detecting pulmonary tuberculosis (PTB) used images acquired from both fluorescence and light microscope [5 - 7]. The specimens are stained using Ziehl-Neelsen (ZN) staining procedure to visualize the bacilli. The automated technique can save the time and cost involved, with reduced human error.

Image contrast and brightness for sputum slide images are among important factors that can affect the accuracy of image analysis process. Microscopic images usually have the problem of low contrast and blurry, which are caused by a couple of factors which have been mentioned earlier. In this paper, image enhancement procedure has been considered for either increasing the image quality, increasing the visibility of TB bacilli or to ease the segmentation process. Modified approaches to perform image enhancement using partial contrast algorithm is presented. The performances of the method are being presented through the resulted image of Ziehl-Neelsen slide after the image enhancement process has been done.



2. Methodology

The aim of partial contrast is to generate an image with higher contrast than the original image. Stretching method is carried out by modifying each pixel value to a new value using pre-specified function. Linear stretching will generally improve the overall contrast of an image. Contrast stretching is a process that applies auto-scaling method, which is a linear mapping function. It is usually used to enhance the brightness as well contrast level of the image. The general mapping function is shown in Equation 1 [8].

$$p_k = \frac{(max - min)}{(f_{max} - f_{min})} (q_k - f_{min}) + min \quad (1)$$

Referring to Equation 1, f_{max} and f_{min} are the maximum and minimum colour level in an input image. max and min are the desired maximum and minimum colour level in the output image. q_k is the colour level of the input pixel while p_k is the colour level of the output pixel. The combination of stretching and compressing process is called partial contrast. A part of the intensity level is being stretched to a new range, while other intensity levels left is being compressed to a different new range as well. The stretching and compressing processes are illustrated by Fig. 1.

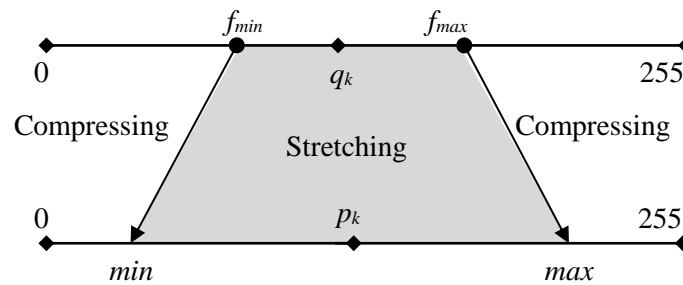


Figure 1: Partial contrast process

The process illustrated by Fig. 1 can be put into a mathematical function such as in Equation 2.

$$p_k = \begin{cases} \frac{min}{f_{min}} (q_k) & ; \text{ for } q_k < f_{min} \\ \frac{(max - min)}{(f_{max} - f_{min})} (q_k - f_{min}) + min & ; \text{ for } f_{min} \leq q_k \leq f_{max} \\ \frac{(255 - max)}{(255 - f_{max})} (q_k - f_{max}) + max & ; \text{ for } q_k \geq f_{max} \end{cases} \quad (2)$$

By applying this technique, the value of pixels within the range of f_{min} and f_{max} will be stretched to a wider new range of min and max . On the other hand, the pixels with values that are outside of this range will be compressed.

In the original algorithm, the technique is meant to be applied to monochrome image that only have one intensity level, which is its greyscale intensity ranging from 0 to 255. However, since the sputum slide images are colour images, modifications need to be made to adopt the original algorithm for implementation on colour images. Colour imaging may be considered as a layered intensity image

processing scheme. This is based on the assumption that each of the colour layers can be processed separately and finally the results are combined. In this study, the process of stretching and compressing for partial contrast technique is implemented as illustrated in Fig. 1.

Each pixel in colour images are represented by three components; red (R), green (G) and blue (B). Therefore, in order to accommodate the algorithm of partial contrast, each parameter in Equation 2 will need to consider for the values from these RGB components. Therefore, the technique is done separately for all three components.

Some modifications have been made to the original partial contrast algorithm to be applied to the sputum slide images. The procedure for implementing partial contrast technique in this study is mentioned as follows:

- i) Read the intensity value of RGB component for each pixel of the original image.
- ii) Develop the RGB histograms for original image using the intensity values obtained.
- iii) Find the intensity value of $f_{min(R)}$, $f_{min(G)}$, $f_{min(B)}$, $f_{max(R)}$, $f_{max(G)}$, $f_{max(B)}$, $min(R)$, $min(G)$, $min(B)$, $max(R)$, $max(G)$ and $max(B)$ for each parameter.
- iv) Perform partial contrast algorithm for each of the RGB component based on Equation 2.
- v) Construct the output image using the combination of RGB components obtained in step (iv).

$f_{min(R)}$, $f_{min(G)}$, $f_{min(B)}$, $f_{max(R)}$, $f_{max(G)}$ and $f_{max(B)}$ are the original images' minimum and maximum values for R, G and B component, respectively. These values are defined by percentage and the real intensity value for each of the parameters will be calculated from the RGB histograms. Meanwhile values of $min(R)$, $min(G)$, $min(B)$, $max(R)$, $max(G)$ and $max(B)$ are the minimum and maximum values for desired intensity level of the output images for R, G and B component respectively.

The real intensity values for parameters $f_{min(R)}$, $f_{min(G)}$, $f_{min(B)}$, $f_{max(R)}$, $f_{max(G)}$ and $f_{max(B)}$ defined in step (iii) of previous procedure are calculated using the steps as follows:

- i) Choose a specific percentage value for each of the specified parameter.
- ii) Initialize the current intensity value to 0.
- iii) Find out the total number of pixels (from the whole image) for each of the specified parameter which is having the current intensity value.
- iv) Sum up the number of pixels obtained in (iii) with the previous summation value (summation value starts with 0).
- v) Calculate the current percentage of the summation value by using Equation 3.

$$\text{current percentage} = \left(\frac{\text{summation}}{\text{total number of pixel}} \right) * 100 \quad (3)$$

- vi) If the result of current percentage is less than the percentage value chosen in (i), increase the current intensity value by 1 and go back to step (iii).
- vii) If the result of current percentage is equal or more than the percentage value chosen in (i), then take the current intensity value as the real intensity value for the specified parameter.

The reason of using percentage value for the parameters is because each of the images has different minimum and maximum intensity level. Therefore, by using percentage value it can ensure that the values to be stretched or compressed are within the range that is suitable to that particular image. On the other hand, if the values to be stretched are fixed, for example 30 for minimum (f_{min}) and 200

for maximum (f_{max}) values, the images that are having a minimum intensity of 60 (min) and maximum intensity of 150 (max) would not experience a complete partial contrast process on its pixels.

In this research, the percentage value for step (iii) that has been chosen for parameters $f_{min(R)}$, $f_{min(G)}$ and $f_{min(B)}$ is 10% while percentage value for $f_{max(R)}$, $f_{max(G)}$ and $f_{max(B)}$ is 90%. These values are chosen because in the RGB histograms of ZN sputum slide images, the values in between these percentage often contains relevant information of TB bacilli, which is the object of interest. Meanwhile the darkest 10% and the brightest 10% of the histograms are usually pixels representing unnecessary objects in the image.

On the other hand, the real intensity value that has been chosen for parameter $min(R)$, $min(G)$ and $min(B)$ is 10 while intensity value for $max(R)$, $max(G)$ and $max(B)$ is 245. After partial contrast, the intensity level for RGB components will be spread out to values between 10 and 245. Fig. 2 illustrates the process of compressing and stretching the pixels to new intensity value.

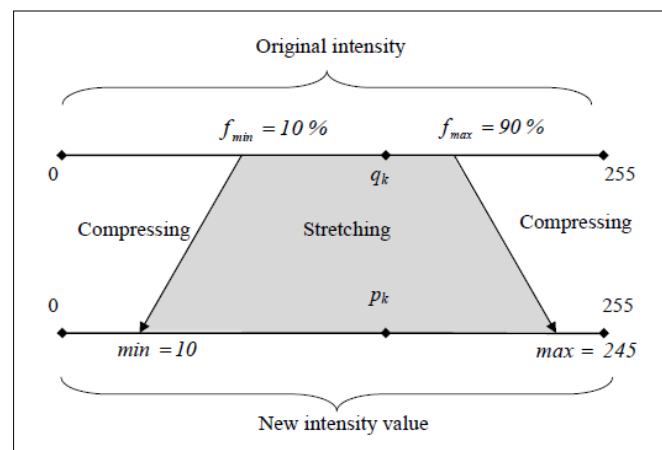


Figure 2: Partial Contrast Technique applied to sputum slide image

The usage of partial contrast technique helps to increase the contrast for images with low contrast. Images can appear too bright if the sputum smear on the specimen slide is too thin at that particular field that is being captured. On the other hand, images can appear darker if the sputum smear on the specimen slide is too thick.

3. Results

Fig. 3 shows the resulted image for partial contrast process together with their histograms.

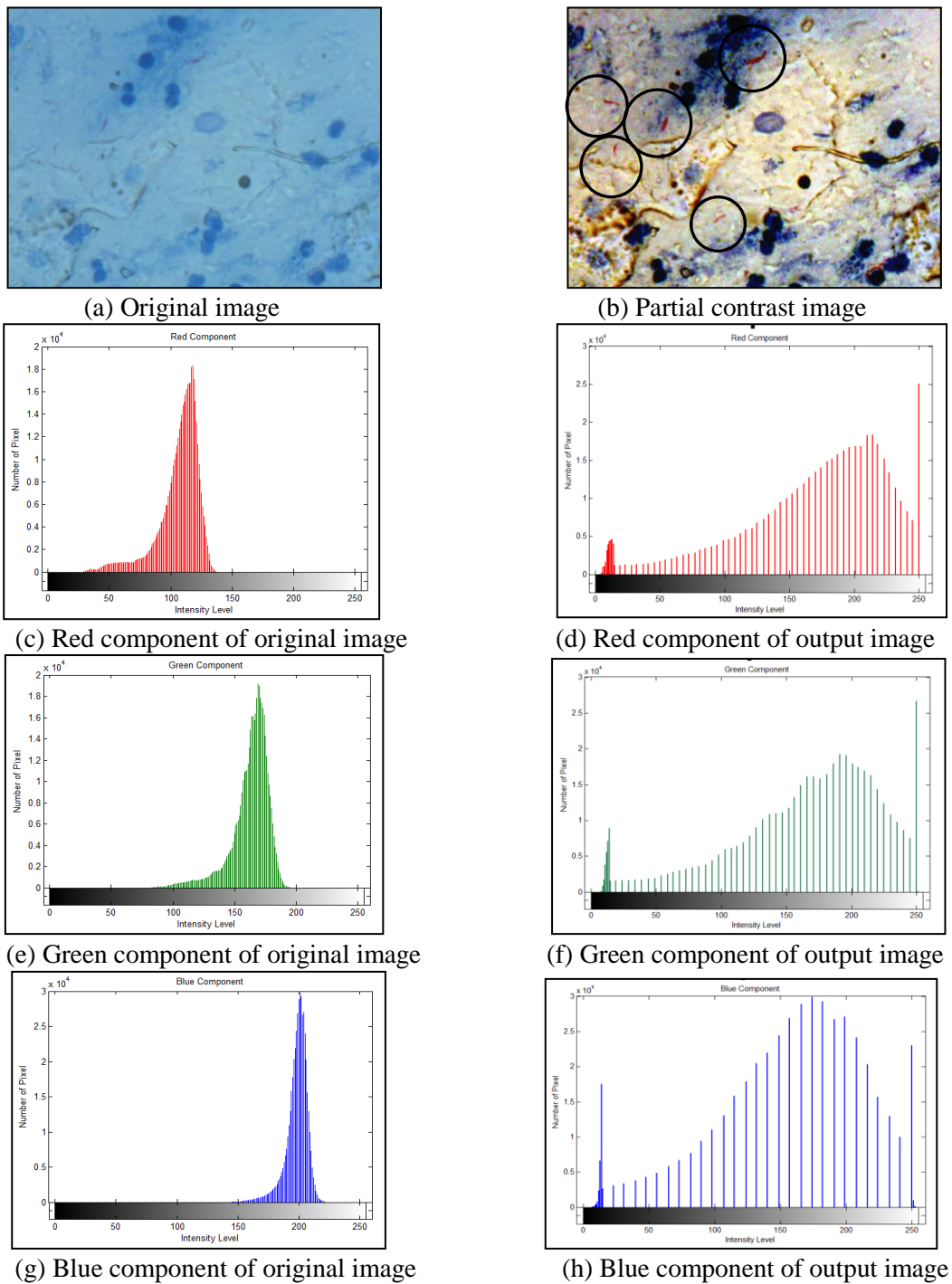


Figure 3: Original Low Contrast Image and Its Partial Contrast Image

Partial contrast has successfully enhanced the contrast of the original image. TB bacilli can be seen clearly in the resulted images compared to the original image. The parameters' value for the particular image shown in Fig. 3(a) are $f_{min(R)} = 85$, $f_{max(R)} = 123$, $f_{min(G)} = 143$, $f_{max(G)} = 178$, $f_{min(B)} = 187$ and $f_{max(B)} = 207$. These are real values that are previously obtained from the percentage values chosen for each parameter. The values have spread out the intensity level of the

image and hence significantly increase the contrast of the image especially the pixels that represents the TB bacilli. The result of partial contrast performed on other low contrast image is shown in Fig. 4.

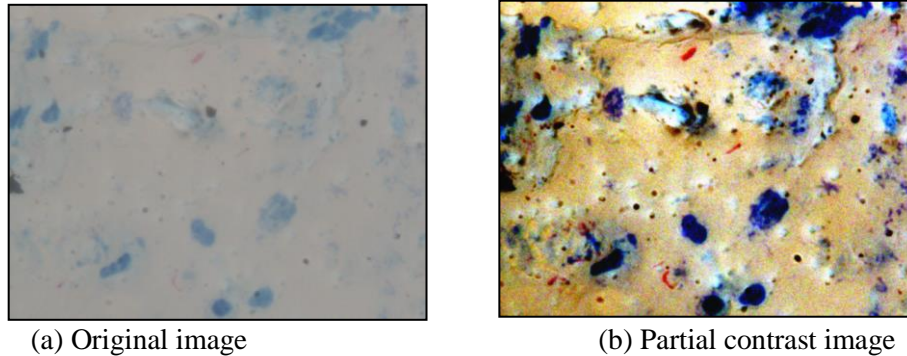


Figure 4: Result of Partial Contrast on Other Image

The resulted pixels from the procedure for each RGB components are combined after the partial contrast process. It can be seen that the contrast in dark pixels increases and thus provides better visual experience. It should be noted that because of this, the colour ratio will change. Hence, the resulted image appearance also will look artificial. However, the object of interest in the image which is the TB bacilli will appear clearer than the original image. This will help the microbiologists and technologists to identify the TB bacilli easily.

4. Conclusion

The modified partial contrast algorithm is proven to be able to increase the contrast range for images with average brightness while lighting up darker images. It also helps to improve TB bacilli visibility. Hence the resulted images would become useful for the microbiologists and technologists for further analysis of ZN sputum slide.

References

- [1] K. Veropoulos, C. Campbell, and G. Learmonth (1998), 'Image Processing and Neural Computing Used in the Diagnosis of Tuberculosis'. Proc. IEE Colloquium on Intelligent Methods in Healthcare and Medical Applications (Digest No. 1998/514), , York, UK.
- [2] K. Veropoulos, C. Campbell, Learmonth, G., B. Knight, and J.Simpson (1998), 'The Automated Identification of Tubercle Bacilli using Image Processing and Neural Computing Techniques'. Proc. 8th International Conference on Artificial Neural Networks, Skövde, Sweden, pp. 797-802.
- [3] Khutlang, R., Krishnan, S., Dendere, R., Whitelaw, A., Veropoulos, K., & Learmonth, G. (2010). Classification of mycobacterium tuberculosis in images of ZN-stained sputum smears. *IEEE Transactions on Information Technology in Biomedicine*, 14(4), 949-957.
- [4] Santiago-Mozos, R., Fernando, P., Michael, G. M., & Antonio, A. (2014). An Automated Screening System for Tuberculosis. *IEEE Journal of Biomedical and Health Informatics*, 18(3), 855-862.
- [5] Cicero F. F. C. F., & Marly, G. F. C. (2012). Sputum Smear Microscopy for Tuberculosis: Evaluation of Autofocus Functions and Automatic Identification of Tuberculosis Mycobacterium. *Understanding Tuberculosis - Global Experiences and Innovative Approaches to the Diagnosis*, 277-292.
- [6] R. Singhal and V. P. Myneedu (2015). Microscopy as a diagnostic tool in pulmonary tuberculosis. *International Journal of Mycobacteriology*, vol. 4, no. 1, pp. 1–6.
- [7] Chang, E. W., Page, A. L. & Bonnet M. (2016). Light-emitting diode fluorescence microscopy for tuberculosis diagnosis: a metaanalysis. *Eur Respir J* 47, 929–937.
- [8] Weeks, J. R. (1996). *Fundamentals of Electronic Image Processing*. Bellingham: SPIE Press.