

HUMAN STRESS LEVEL COMPUTATION USING MULTIPLE PHYSIOLOGICAL SIGNALS - BASED ON FUSION TECHNIQUE THROUGH DYNAMIC BAYESIAN NETWORK

KARTHIKEYAN PALANISAMY (1040610461)

by

cted

A thesis submitted in fulfillment of the requirements for the degree of Doctor of Philosophy

> School of Mechatronic Engineering UNIVERSITI MALAYSIA PERLIS

> > 2014

UNIVERSITI MALAYSIA PERLIS

	DECLARATION OF THESIS
Author's full name :	KARTHIKEYAN PALANISAMY
Date of birth	20/ 05/ 1985
THe	HUMAN STRESS LEVEL COMPUTATION USING MULTIPLE PHYSIOLOGICAL
	SIGNALS - BASED ON FUSION TECHNIQUE THROUGH DYNAMIC BAYESIAN
	NETWORK
Academic Session :	2012 - 2013
I hereby declare that the the at the library of UniMAP. Thi	is thesis is classified as :
	(Contains confidential information under the Official Secret Act 1972)*
	(Contains restricted information as specified by the organization where research was done)
OPEN ACCESS	I agree that my thesis is to be made immediately available as hard copy or on-line open access (full text)
I, the author, give permission research or academic excha	on to be UniMAP to reproduce this thesis in whole or in part for the purpose of insponly (except during a period of years, if so requested above).
item	Certified by:
SIGNATUR	E SIGNATURE OF SUPERVISOR
(NEW IC NO. / PAS	SPORT NO.) NAME OF SUPERVISOR
	Data :

NOTES : * If the thesis is CONFIDENTIAL or RESTRICTED, please attach with the letter from the organization with period and reasons for confidentially or restriction.

ACKNOWLEDGMENT

First and Foremost, I would like to express my sincere gratitude to Prof. Dr. Sazali Yaacob and Dr.M.Murugappan for their valuable supervision, professional guidance, and financial support in this research. Their patience and positive attitudes stand-in me to complete the PhD thesis.

I would like to express my sincere and profound gratitude to the Vice Chancellor of University Malaysia Perlis, Y. Bhg. Brigedier Jeneral Datuk' Prof. Dr. Kamarudin B. Hussin for granting me permission to study in this university.

A special thanks to the Dean of School of Mechatronic Engineering, University Malaysia Perlis, Prof. Dr. Abdul Hamid Adom for providing support during my research work.

My sincere thanks to Prof Dr. Mohd Yusoff Mashor, Dean of Centre of Graduate Studies (CGS), staff members of CGS and Dr.Cheng Ee Meng, Postgraduate Chairman, School of Mechatronics Engineering for their concern and help during the study. It is my duty to express the acknowledgement to Lim Wei Ling, Nithiyakalyani, Puvaniswaran and Bong Siao Zheng for arranging the subjects and thankful to the subjects voluntarily participated in data acquisition and pilot study of this research.

I would also like to thank my family for the support provided me through my entire life and in particular, my parents Palanisamy and Saroja and my siblings Vellaichamy, Sellappandian and Gandhi Arumugam for their love, continuous support, and encouragement in completing this research work.

I am grateful to Prof.Dr. Ulf Lundberg, Department of Psychology, Stockholm University, Dr.Gari D.Clifford, Department of Engineering Science, University of Oxford and Prof.Dr. Wolfgang Linden, Department of Psychology, University British Columbia for their suggestions, materials and communication during this research.

In conclusion, I am deeply thankful to different divinities existing in the universe by the principal concept of belief for successfully completing the research.

TABLE OF CONTENT

			PAGE
DEC	LARAT	ION	i
ACK	NOWL	EDGEMENT	ii
ТАВ	LE OF	CONTENTS	iii
LIST	T OF TA	BLES	Х
LIST	OF FI	GURES	xii
LIST	COFAB	BREVIATION	xvii
ABS	TRAK (BM)	xxii
ABS'	TRACT	(ENGLISH)	xxiii
СНА	PTER 1	INTRODUCTION	
1.1	Overvi	ew of Human Stress	1
1.2	Proble	m in Human Stress Computation	5
1.3	Resear	ch Objectives	6
1.4 (Thesis	Organization	7
СНА	PTER 2	2 DEVELOPMENTS ON HUMAN STRESS COMPUTATION	1
2.1	Introdu	iction	9
2.2	Humar	n Stress	9
	2.2.1	Effects of Stress on Human Function System	9
	2.2.2	Different Types of Human Stress	11
2.3	Humar	Stress and its Levels Computation Methods and Approaches	13

	2.3.1	Psychophysiological Questionnaires Based Human Stress Identification	14
	2.3.2	Human Stress Computation in Real-Time Task	15
	2.3.3	Computation of Stress Using Stimuli (Laboratory Stressor)	16
2.4	Compu	tational Measures Investigated in Human stress	24
	2.4.1	Biochemical Samples Based Invasive Approach	24
	2.4.2	Invasive and Noninvasive Approach using Physiological Signals	25
	2.4.3	Importance of Multiple Physiological Signals in Computation of Stress	34
	2.4.4	Justification on Selection of Physiological Signals	35
2.5	Physiol	ogical Signal Processing in Computational Study	36
	2.5.1	Noise Removal Methods for Processing the Physiological Signals	36
	2.5.2	Feature Extraction Methods of Physiological Signals	37
	2.5.3	Frequency Band Localization for Stress Identification through Physiological Signals	41
	2.5.4	Stress Related Features in Multiple Physiological Signals	42
	2.5.5	Statistical Methods Involved in the Analysis of Human Stress	43
2.6	Classifi	cation of Human Stress and its Levels Using Physiological Signals	44
(2.6.1	Issues in Classification of Multiple Physiological Features	47
2.7	Fusion	Models for Uncertainty Problems in Real World Task	48
2.8	Probabi	listic Methods Involved in Data Fusion	49
	2.8.1	Hidden Markov Model	50
	2.8.2	Dynamic Bayesian Network	51
2.9	Signific	cant Observations of Review for Stress Level Computation	52
2.10	Summa	ry	54

CHAPTER 3 DEVELOPMENT OF STRESS INDUCING PROTOCOL AND DATA COLLECTION

3.1	Introduction	55
3.2	Overview of Developed Methodology for Human Stress Level Computation Using Multiple Physiological Signals	55
3.3	Empirical Setup of Data Acquisition and its Environment	58
3.4	Protocol Design of Computerized Mental Arithmetic Task Based Stress- Inducing Stimuli	59
	3.4.1 Significance of Computerized Mental Arithmetic Task	61
3.5	Information about Data Acquisition Instruments	61
3.6	Participated Human Subject's Information	62
3.7	Multi-Electrode Placements for Physiological Signal Acquisition	63
3.8	Description of Multiple Physiological Signals Human Stress Dataset	65
3.9	Origins and Characteristics of Multiple Physiological Signals Investigated	65
	3.9.1 Cardiac System (Electrocardiogram and Heart Rate Variability)	66
	3.9.2 Muscular System (Electromyogram)	68
	3.9.3 Integumentary System (Galvanic Skin Response and Skin Temperature)	69
3.10	Self-Assessment Questionnaires	72
	3.10.1 Questionnaire's for Recalling the Previous Stressful Experience	72
	3.10.2 Subject Feedback Questionnaire about the Stress-Inducing Task	73
3.11	Summary	73

CHAPTER 4 PHYSIOLOGICAL SIGNAL PROCESSING FOR HUMAN STRESS LEVEL CLASSIFICATION

4.1	Introduction	74
4.2	Operational Description of Signal Processing	74

4.3	Wavele (EMG)	t Denoising for Electrocardiogram (ECG) and Electromyogram Noises Removal	77
	4.3.1	Use of Discrete Wavelet Transform in Denoising	78
	4.3.2	Wavelet Filters on Denoising	79
	4.3.3	Hard Thresholding and Soft Thresholding Methods	80
	4.3.4	Thresholding Rules	81
	4.3.5	Wavelet Denoising Algorithm	83
4.4	HRV Si	gnal Extraction from ECG and its Artifacts Removal	84
	4.4.1	Coif 5 Wavelet Function Based HRV Signal Extraction	85
	4.4.2	Ectopic Beat Removal of HRV	87
4.5	Digital Temper	Elliptic Filtering for Galvanic Skin Response (GSR) and Skin ature (ST) Signals' Noise Removal	88
4.6	Discrete	e Packet Wavelet Transform (DWPT)	90
	4.6.1	DWPT for Time and Frequency Domain Extraction and Analysis	90
	4.6.2	Characteristics of Coif 5 Wavelet Function	93
	4.6.3	Algorithm for Extracting Frequency Bands through DWPT	94
4.7	Validati	on and Feature Extraction of Unevenly Sampled Short-Term HRV	101
	4.7.1	Hypothesis of HRV Signals Analyses in Short-Time Durations	101
(4.7.2	Evenly Sampled HRV Signal Power Spectral Information Extraction of Using Fast Fourier Transform (FFT)	103
	4.7.3	Power Spectral Information Extraction of Unevenly Sampled HRV Signal Using LS Periodogram	106
4.8	Automa	tic Startle Detection Algorithm of GSR Signal	108
4.9	Descrip	tion of Various Features Investigated	109
4.10	Normal	ization of Features	115
4.11	Nonline	ear Classifier	116
	4.11.1	K Nearest Neighbor (KNN)	116

	4.112	Probabilistic Neural Network (PNN)	117
	4.11.3	Support Vector Machine (SVM)	119
	4.12.4	Features Treatment for Improve the Performance of Classification	122
4.12	Statistic	al Analysis using One-Way ANOVA	124
4.13	Summa	ry	125

CHAPTER 5 DYNAMIC BAYESIAN NETWORK BASED MULTIPLE PHYSIOLOGICAL INFORMATION FUSION

5.1	Introdu	ction Q	126
5.2	Inform	ation Fusion	126
	5.2.1	Fusion Technique	127
	5.2.2	Fusion Methods	128
	5.2.3	Issues on Different Characteristics of Fusible Information	130
5.3	Probab	ilistic Model	129
	5.3.1	Hidden Markov Model (HMM)	131
	5.3.2	Dynamic Bayesian Network (DBN)	132
	5.3.3	Significance Difference between DBN and HMM	134
5.4	Variab	le-Order HMM Based DBN for Human Stress Level Computation	135
	5.4.1	Semantic of Variable-Order HMM Based DBN	139
	5.4.2	Forward-Backward Procedure (Baum-Welch)	143
	5.4.3	Conditional Dependencies	145
	5.4.4	Boundary Optimization Individual Features	146
	5.4.5	Inference of Information Propagation with Conditional Dependencies	148
	5.4.6	Maximum likelihood Estimation (MLE)	149
	5.4.7	Inference of Significant Feature Vectors using DBN	149

5.5	Multipl Stress L	e Physiological Signal's Multi-Features Decision level Fusion in Level Computation	153
5.6	Perform	nance Measures	159
5.7	Summa	ry	162
СНА	PTER 6	RESULTS AND DISCUSSION	
6.1	Introdu	iction	163
6.2	Questio	onaries' Based Analysis	163
	6.2.1	Subject Response to the Questionnaire in the Living Environment	163
	6.2.2	Subject Response to the Questionnaire about Stress-Inducing Task	165
6.3	Perform	nance of Multiple Physiological Signals in Preprocessing	166
	6.3.1	Wavelet Denoising of ECG Signal	166
	6.3.2	Wavelet Denoising of EMG Signal	168
	6.3.3	Spectral Information Changes in HRV Signal by Applying the Ectopic Beat Removal Procedure	170
	6.3.4	Power Spectral Analysis of GSR and ST Signals in Preprocessing	171
6.4	Classif Physio	ication and Identification of Dominant Features in the Multiple logical Signals for Stress Level Computation	173
	6.4.1	Feature Extraction Module of Time and Frequency Domain	173
(6.4.2	Classification Module for Dominant Features Identification	175
	6.4.3	Identification of Dominant Features in ECG Signal	177
	6.4.4	Identification of Dominant Features in HRV Signal	182
	6.4.5	Identification of Dominant Features in EMG Signal	189
	6.4.6	Identification of Dominant Features in GSR and ST Signal	196
6.5	Discus Compu	sion on Multiple Physiological Signal Based Human Stress Level atation	200
6.6	Results and Bo	s of Dynamic Bayesian Network Based Feature Vector Optimization bundary Estimation	206

	6.6.1	Learning of ECG Signal Features	207
	6.6.2	Learning of HRV Signal Features	210
	6.6.3	Learning of EMG Signal Features	214
	6.6.4	Learning of GSR and ST Signals Features	217
6.7	Results Fusion	s of Multiple Physiological Signal's Multi-Features Decision Level	219
6.8	Discuss	sion on Dynamic Bayesian Network Decision Level Fusion	228
6.9	Summa	ary	230
CHA	PTER 7	CONCLUSION AND FUTURE WORK	
7.1	Conclus	sion	232
	7.1.2	Significant Contribution obtained in Stress Level Computation Using Multiple Physiological Signals	233
	7.1.3	Improvements in Various Stages of the Stress Level Computation Methodologies	235
7.2	Recomr Comput	nendation for Further Advancement to Human Stress Level tation Research	238
RFEF	RENCES		240
APPE		N ^{CC}	250
APPE	ENDIX I	3	252
APPE	endix (C	256
APPE	ENDIX I)	266

LIST OF TABLES

NO		PAGE
2.1	Stress level estimation using Holmes & Rahe questionnaires	14
2.2	Previous works of mental arithmetic task in human stress assessment	18
2.3	Previous works of Stroop colour word test in human stress assessment	22
2.4	Review of stress identification methods	30
2.5	Physiological signals and their suitability as indicators of stress	34
2.6	Responses of physiological signals to acute and chronic stress	34
2.7	Selection of physiological signals for stress level computation	36
2.8	Stress detection and its level classification methods	45
3.1	Information of multiple physiological based stress dataset using mental arithmetic task	66
3.2	Typical values of galvanic skin response	70
4.1	Sampling frequency distribution in HRV	102
4.2	Minimum time duration required to analyze the LF and HF bands in HRV signal	102
4.3	Short-term HRV and number of beats related to HF and LF bands	103
4.4	List of frequency bands and features investigated	110
4.5	Investigated features in HRV signal's time domain	111
4.6	Onvestigated features in ECG, EMG, and HRV signals	112
5.1	Contextual variables	150
5.2	Observational variable with respect to contextual variables	150
5.3	Confusion matrix to compute the performance measures of four-class problem	160
6.1	Stress boundaries for self-developed questionnaire	164
6.2	Results of questionnaires based stress-inducing factors detection	164
6.3	Confusion matrix of the subject response to questionnaire	165
6.4	Statistical information before and after removal of ectopic beat	170

6.5	Statistical analysis of ECG signal's features between four levels of stress	181
6.6	Statistical analysis of HRV signal's features between four levels of stress	187
6.7	Statistical analysis of EMG signal's features between four levels of stress	194
6.8	Statistical analysis of GSR and ST signals features between four levels of stress	198
6.9	Results of Dominant features in multiple physiological signal based stress level computation	201
6.10	Comparative analysis of previous works to present human stress level computation	203
6.11	ECG signal DBN outputs, MLE, upper, and lower bounds with 95% confidence interval	209
6.12	HRV signal DBN outputs, MLE, upper, and lower bounds with 95% confidence interval	212
6.13	EMG signal DBN outputs, MLE, upper, and lower bounds with 95% confidence interval	215
6.14	GSR and ST signals DBN outputs, MLE, upper, and lower bounds with 95% confidence interval	218
6.15	Generalized boundary 1 and its statistical results	221
6.16	Generalized boundary 2 and its statistical results	223
6.17	Generalized boundary 3 and its statistical results	223
6.18	Results of Fusion using KNN classifier	226
6.19	Results of fusion using PNN classifier	228
6.20	Results of fusion using SVM classifier	228

LIST OF FIGURES

NO		PAGE
1.1	Scheme of human stress identification research	3
2.1	A model of various external factors induces the stress on human	10
2.2	Human Stress pathway	10
2.3	Types of stress	12
2.4	Model of general adaptation syndrome in stress	13
2.5	Stroop's first experiment on stress inducement	20
2.6	Stroop's second experiment on stress inducement	20
2.7	Stress pathway and physiological sensors placement on human function system	26
3.1	Outline of proposed methodology to compute the stress level	56
3.2	Photograph of experimental setup	58
3.3	Protocol layout of computerized mental arithmetic task	59
3.4	Images of data acquisition accessories used in this work	62
3.5	Information of the participated subjects	63
3.6	Multiple physiological sensors electrode placements	64
3.7	Acquired and derived multiple physiological signal patterns	65
3.8	ECG signal originated from different nodes	67
3.9	Einthoven triangle placement for ECG signal pick up	68
3.10	Electrode placement on Trapezius and origin of EMG Signal	69
3.11	Origin of GSR signal and its electrode configuration	71
3.12	Electro dermal response of GSR signal	70
4.1	Schematic description of various methods involved stress level computation	76
4.2	Decomposition of signal in DWT	80

4.3	Thresholding methods in wavelet denoising	81
4.4	Wavelet denoising algorithm using thresholding technique	84
4.5	HRV signal detection algorithm using coif 5 function based modified Pan Tompkins algorithm	86
4.6	HRV signal detection process from ECG signal	87
4.7	Fourth order elliptic filter magnitude and phase response	89
4.8	Vector subspace representation of wavelet packets	92
4.9	Decomposition of DWPT and cutoff frequency in each level	93
4.10	Coif5 wavelet function in decomposition and reconstruction	94
4.11	Algorithm for Extracting Frequency time and frequency bands using DWPT	95
4.12	Wavelet packet selections for extracting required frequency bands of ECG signals	97
4.13	Time and frequency domain extraction of (0-10) Hz	97
4.14	Time and frequency domain extraction (0.04-0.14) Hz	98
4.15	Time and frequency domain extraction (0.15-0.5) Hz	98
4.16	Wavelet packet selections for extracting required frequency bands of EMG signals	99
4.17	Time and frequency domain extraction of (0-15) Hz	100
4.18	Time and frequency domain extraction of (0-0.03) Hz	100
4.19	Time and frequency domain extraction(0-0.8) Hz	100
4.20	Frequency spectrum of HRV signals	101
4.21	HRV signal on each stages of feature extraction	107
4.22	HRV signal on each stages feature extraction	107
4.23	Startle detection algorithms for GSR signal feature extraction	109
4.24	Features in electro dermal responses of GSR signal	114

4.25	KNN decision dependency respect on K value	117
4.26	Architecture of PNN classifier for four classes	118
4.27	Linear and nonlinear separable boundaries of SVM classifier using linear kernel	120
4.28	Data handling in nonlinear classifiers	123
4.29	Different hypotheses using one-way ANOVA	124
5.1	Multiple sensors parallel information's fusion model	127
5.2	Different types of multi-sensorial information fusion model	129
5.3	A simple Bayesian model	133
5.4	The simple Bayesian interference grass wet Vs. cloud	134
5.5	Probabilistic framework multiple physiological signals' information fusion using variable-order HMM based DBN	137
5.6	Variable order-HMM based DBN for significant feature extraction and generalization of decision boundary	138
5.7	Variable-order HMM in the network	140
5.8	Variable-order HMM Based DBN Model	143
5.9	Forward and backward procedure used in DBN model	144
5.10	A valid DBN information propagation in different modes	145
5.11	Information propagation with conditional dependency and contextual	
	evidence	148
5.12	Inference of stress level computation using the DBN	151
5.13	Conditional dependency of different nodes	152
5.14	Multiple physiological signal based fusion	156
5.15	Performance measures and its different characteristics	159
6.1	Decomposed and denoised signal coefficients in each level of ECG	
	signal	167

6.2	Power spectral density of raw and preprocessed ECG signal	167
6.3	Decomposed and denoised signal coefficients in each level of EMG signal	169
6.4	Power spectral density of raw and preprocessed EMG signal	169
6.5	Ectopic beat and its removal through ectopic beat removal algorithm	171
6.6	Preprocessing response of GSR signal	172
6.7	Preprocessing response of ST signal	172
6.8	Multiple physiological signal based human stress level computation- feature extraction module	174
6.9	Multiple physiological signal based human stress level computation- classification and dominant features optimization module	176
6.10	ECG signal's dominant features F_1 score for stress level classification in three nonlinear classifiers	179
6.11	Maximum average classification accuracy and precision of ECG signal's dominant features	180
6.12	Mean value changes of optimized ECG features in various stress levels with trend lines	181
6.13	HRV signal's dominant features F_1 score for stress level classification in three nonlinear classifiers	184
6.14	Maximum average classification accuracy and precision of HRV signal's heart rate and LF band dominant features	185
6.15	Maximum average classification accuracy and precision of HRV signal's HF band dominant features	186
6.16	Dominant features of HRV signal heart rate (time domain) and HF band mean value and its characteristics of various levels	188
6.17	Dominant features of HRV signal HF band mean value and its characteristics of various levels	188
6.18	EMG signal's dominant features F_1 score for stress level classification in three nonlinear classifiers	191
6.19	Maximum average classification accuracy and precision of EMG signal's dominant features	193
6.20	EMG signal frequency domain mean value of each state	195

6.21	EMG signal time domain mean value of each state	196
6.22	GSR and ST signals dominant features F_1 score for stress level classification in three nonlinear classifiers	197
6.23	Maximum average classification accuracy and precision of GSR and ST signals dominant features	198
6.24	Statistical characteristics of GSR and ST signals dominant features	199
6.25	MLE, confidence interval and probability density function of ECG signal frequency domain (0.04-0.14) Hz mean feature	207
6.26	ECG signals Bayesian probability of each feature in different levels	208
6.27	Dispersion of significant feature vectors obtained in DBN using ECG signal's dominant features	210
6.28	HRV signals Bayesian probability of each feature in different levels	211
6.29	Dispersion of significant feature vectors obtained in DBN using HRV signal's dominant features	213
6.30	EMG signals Bayesian probability of each feature in different levels	214
6.31	Dispersion of significant feature vectors obtained in DBN using EMG signal's dominant features	216
6.32	GSR and ST signals Bayesian probability of each feature in different levels	217
6.33	Dispersion of significant feature vectors obtained in DBN using GSR and ST signals dominant features	218
6.34	Three different generalized boundaries obtained through DBN that originated from the 5 physiological sensor over the 20 features	224
6.35	\mathbf{F}_1 score and standard error of kappa in fusion without transformation	225
6.36	F ₁ score and standard error of kappa in fusion with transformation	227

LIST OF ABBREVIATION

- AAD Average absolute deviation
- ANOVA Analysis of variance
- ANS Autonomic nervous system
- AR Auto regressive
- by original copyright ARMA Auto regressive moving average
- ATH Adrenal hypothalamus
- BMI Body mass index
- BP Blood pressure
- BVP Blood volume pulse
- CA Approximation coefficient
- CAD Coronary artery disease
- CD Detailed coefficient
- CPD Conditional probability distribution
- Continuous wavelet transform CWT
- DAG Directed acyclic graph
- Depression anxiety stress scale DASS
- DBN Dynamic Bayesian network
- DBP Diastolic blood pressure
- DFA Detrended fluctuation analyses
- DST Dempster Shaffer theory
- DFT Discrete Fourier transform
- Discrete wavelet packet transform DWPT
- DWT Discrete wavelet transform
- ECG Electrocardiogram

- EDA Electro dermal activity
- EEG Electroencephalogram
- EMD Empirical mode decomposition
- EMG Electromyography
- A by original copyright ENATF European and north American task force
- FD Frequency domain
- FFT Fast Fourier transform
- FN False negative
- FOD First order difference
- FP False positive
- Fisher projection matrix FPM
- GAS General adaptation syndrome
- Galvanic skin response GSR
- Hilbert Huang transform HHT
- HMM Hidden Markova model
- HOS Higher order statistics
- HPF High pass filter
- HR Heart rate
- HRV Heart rate variability
- HRVTI HRV Triangular Index
- IAV Integral of absolute value
- IBI Inter-beat-interval
- Irritable bowel syndrome IBS
- ICA Independent component analysis

- **IDWPT** Inverse discrete wavelet packet transform
- IDWT Inverse discrete wavelet transform
- IIR Infinite impulse response
- VLF very low frequency
- WPC
- WPT
- IS
- KNN
- .criminate analysis .criminate analysis Low frequency Low pass differential Low pass filter omb-Scarg¹, LDA
- LF
- LPD
- LPF
- LS
- Median absolute deviation MAD
- MAT Mental arithmetic task
- MF Mid-frequency
- MLE Maximum likelihood Estimation
- MLP Multi-layer perceptron
- MSE Mean square error
- NLP Natural language processing
- PD Pupil diameter
- PDF Probability density function
- PN Probabilistic network
- PNN Probabilistic neural network

- PNS Parasympathetic nervous system
- PSD Power spectral density
- OP Quadratic programming
- QCD Quartile coefficient of dispersion
- RBF Radial-bias function
- by original copyright RMSSD Root mean square of the standard deviation
- RR **Respiration rate**
- RS Resting segment
- SAIL Smart assisted in living
- Self-analysis questionnaire SAQ
- Static Bayesian networks SBN
- Systolic blood pressure SBP
- Skin conductance level SCL
- Standard error SE
- **SNR** Signal-to-noise ratio
- **SNS** Sympathetic nervous system
- SRR Skin resistance response
- ST Skin temperature
- STFT Short-term Fourier transform
- Steins unbiased risk estimator SURE
- SV Stroke volume
- Support vector machine SVM
- TD Time domain
- TP True positive

- very low frequency VLF
- Trier social stress test TSST
- Weighted low pass differential WLPD
- WPC wavelet packet coefficients
- WT
- ZC

o this term is protected by original copyright

Pengiraan Aras Tekanan Manusia Menggunakan Pelbagai Isyarat Fisiologi -Berdasarkan Teknik Fusion melalui Rangkaian Dynamic Bayesian

ABSTRAK

Tesis ini mengkaji untuk meningkatkan pengiraan aras tekanan dan kebolehpercayaan dengan menggunakan pelbagai isyarat fisiologi. Dalam tesis ini, penginduksian tekanan, pengambilalihan isyarat fisiologi, prapemproses, pengekstrakan ciri, klasifikasi, pengoptimuman ciri-ciri dari pelbagai isyarat fisiologi, anggaran ciri penting, pengoptimuman keputusan sempadan dan gabungan adalah langkah-langkah penting yang terlibat. Tugas mental aritmetik rangsangan telah digunakan untuk mendorong tekanan pada 60 subjek yang sihat dengan umur purata 22.5 ± 2.5 tahun. Lima jenis isvarat fisiologi diambilkira dalam penviasatan ini (elektrokardiogram (ECG), eelectromyogram (EMG), response kulit galvani (GSR), suhu kulit (ST), kepelbagaian kadar jantung (HRV)) untuk mengukur kesan dorongan tekanan pada subjek. Isyarat ECG dan EMG yang diperoleh telah dipraproses dengan menggunakan kaedah 'wavelet denosing' untuk menyingkirkan bunyi dalam keseluruhan julat frekuensi isyarat dan penapis perintah keempat eliptik digital digunakan untuk menyingkirkan bunyi dalam isyarat GSR dan ST. Algoritma penyikiran ektopik digunakan untuk menghapuskan kehadiran puncak bunyi dan artifak dalam isyarat HRV. Dalam pengekstrakan ciri, ciri-ciri isyarat ECG dan EMG dikira menggunakan diskret wavelet packet transform (DWPT) dan Lomb-Scargle (LS) periodogram telah digunakan untuk mengeluarkan spectrum kuasa rendah dan jalur frekuensi yang tinggi dalam isyarat istilah pendek HRV. Algoritma pengesanan ketakutan telah dilaksanakan untuk mengeluarkan dan menganalisis ciri-ciri yang berkaitan dengan GSR tonik tindak balas, dan akhirnya ciri-ciri suhu kulit diekstrak secara langsung dalam rantau masa. *Ciri-ciri yang diperolehi telah dikelaskan kedalam empat tahap tekanan termasuk tahap* normal dengan menggunakan tiga pengelas linear (K paling hampir neighbor (KNN), rangkaian neural berkebarangkalian (PNN), dan mesin vektor sokongan (SVM)). Kadar klasifikasian purata dan skor F_1 melebihi 50% dan 0.5 dianggap sebagai ciri dominan dalam kerja ini. Keputusan menunjukkan 20 ciri sebagai dominan dikalangan 244 ciri-ciri yang disiasat dalam pelbagai jalur frekuensi lima isyarat fisiologi. Purata maksimum ketepatan klasifikasi empat peringkat telah diperoleh 74.20% dalam ciri min ECG 74.75% dalam ciri cumulant ketiga HRV, 74.67% dalam min EMG, 66.84% dalam cirri kekerapan ketakutan daripada GSR, dan 63.63% dalam ciri min ST dalam kajian hal bebas. Bagi meningkatkan kadar klasifikasi tahap tekanan dan kebolehpercayaanya, pengoptimuman sempadan keputusan dan ciri fisiologi penting vector anggaran diperlukan. Pemboleh ubah-perintah tersembunyi Markova model (HMM) berdasarkan rangkaian Bayesian dinamik (DBN) telah dibina untuk mendapatkan perubahan dinamik setiap ciri isyarat fisiologi dan berupaya untuk mengenalpasti vektor ciri penting dan sempadan keputusan sepadan dengan pelbagai tahap tekanan. Rangkaian DBN yang mengamkan tiga sempadan keputusan yang terdiri daripada 20 ciri-ciri berbeza yang diproses, dan hasilnya menunjukkan bahawa purata kebarangkalian Bayesian maksimum untuk setiap sempadan adalah 0,544, 0.61 dan 0.75 dalam semua keadaan berkenaan kepada keadaan normal. Akhirnya, vektor ciri-ciri yang dioptimumkan ini menjadi milik sempadan yang berbeza dan telah digabungkan untuk membuat keputusan global dengan ketepatan pengesanan yang lebih baik dan boleh dipercayai.

Human Stress Level Computation Using Multiple Physiological Signals-Based on Fusion Technique through Dynamic Bayesian Network

ABSTRACT

This study investigates to improve the stress levels computation and its reliability using multiple physiological signals. In which, stress inducement, physiological signal acquisition, preprocessing, feature extraction, classification, optimization of features from multiple physiological signals, significant feature estimation, decision boundary optimization, and fusion are the major process. Mental arithmetic task stimulus is used to induce stress on the subjects and sixty healthy subjects with a mean age of 22.5 ± 2.5 years were used. This investigation considered the five physiological signals (electrocardiogram (ECG), heart rate variability (HRV) signal, electromvogram (EMG), galvanic skin response (GSR), and skin temperature (ST)) to measure the effect of stress induced on the subject. The acquired ECG and EMG signals were preprocessed using wavelet denoising method to remove the noises in the frequency range of signals and 4th order IIR elliptic filter to remove the noises in GSR and ST signals. The ectopic beat removal algorithm was used to eliminate the presence of noise peaks and artifacts in HRV signal. In the feature extraction, ECG and EMG signals features were computed using discrete wavelet packet transform (DWPT), Lomp-Scargle (LS) periodogram is used to extract the low and high frequency band's power spectrum in the short- term HRV signal. The startle detection algorithm was implemented to extract and analyze the feature related to GSR tonic response, and finally the skin temperature features were extracted directly in the time domain. The obtained features classified in to four levels of stress including normal using three nonlinear classifiers (K nearest neighbor (KNN), probabilistic neural network (PNN), and support vector machine (SVM)). Average classification rate and F_1 score above 50% and 0.5 are considered as the dominant features respectively in this work. Result indicates that, 20 features as dominant features among the 244 features investigated over various frequency bands of five physiological signals. The maximum average classification accuracy of four levels was obtained as 74.20% in mean feature of ECG, 76.69% in third cummulant feature of HRV, 74.67% in mean of EMG, 66.84% in startle frequency feature of GSR, and 63.63% in mean feature of ST in subject-independent study. The results also indicate a significant improvement of classification results in the four class of subject-independent study over the earlier highly subject-dependent studies. In order to improve the classification rate on stress levels and its reliability, the optimization of decision boundary based on physiologically significant feature vectors estimation is required. The variable-order hidden Markov model (HMM) baseddynamic Bayesian network (DBN) was constructed to extract the dynamic changes of each physiological signal feature and capable to identify the significant feature vectors and decision boundaries corresponding to the different levels of stress. The DBN networks generalized the three decision boundaries of the 20 different dominant features processed, and the result shows that the maximum average Bayesian probability of each boundary is 0.544, 0.61, and 0.75 in all the states with respect to normal state. Finally, these optimized feature vectors belongs to different boundaries fused to make the global decision to ensure the reliability. The result shows that, an excellent agreement of reliability measure with improved classification accuracy while the significant components only presents in the fusion.